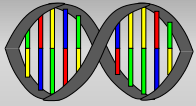


# ***The Dynamics of Excitability***

J. P. Keener

Mathematics Department

University of Utah

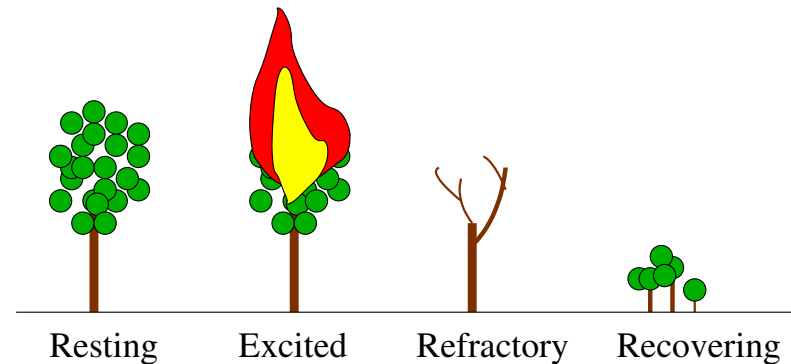


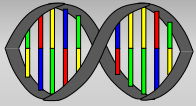
# Examples of Excitable Media

- B-Z reagent
- Nerve cells
- cardiac cells, muscle cells
- Slime mold (*dictyostelium discoideum*)
- CICR (Calcium Induced Calcium Release)
- Forest Fires

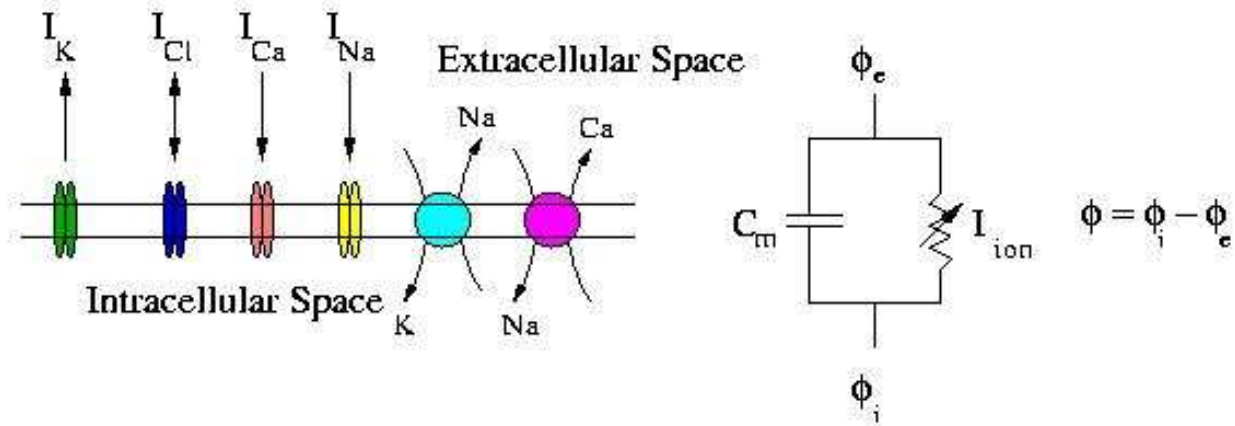
## Features of Excitability

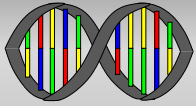
- Threshold Behavior
- Refractoriness
- Recovery



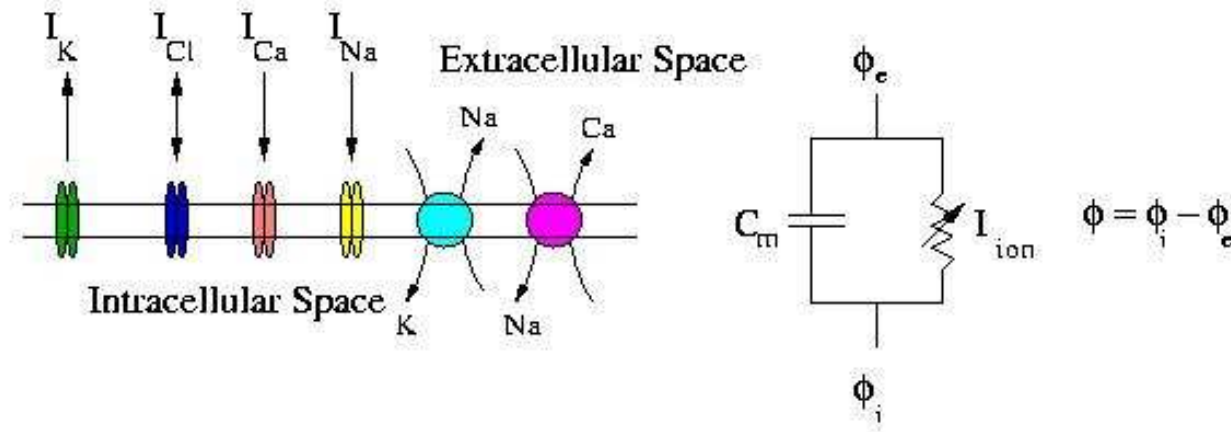


# Modeling Membrane Electrical Activity



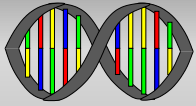


# Modeling Membrane Electrical Activity



Transmembrane potential  $\phi$  is regulated by transmembrane ionic currents and capacitive currents:

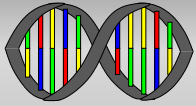
$$C_m \frac{d\phi}{dt} + I_{ion}(\phi, w) = I_{in} \quad \text{where} \quad \frac{dw}{dt} = g(\phi, w), \quad w \in R^n$$



# Examples

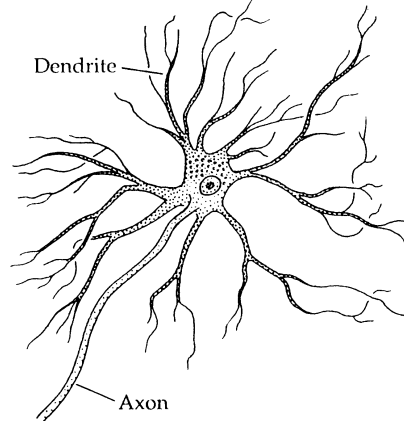
Examples include:

- Neuron - **Hodgkin-Huxley model**
- Purkinje fiber - Noble
- Cardiac cells - Beeler-Reuter, Luo-Rudy, Winslow-Jafri, Bers
- Two Variable Models - **reduced HH, FitzHugh-Nagumo, Mitchell-Schaeffer, Morris-Lecar, McKean, Puschino, etc.)**

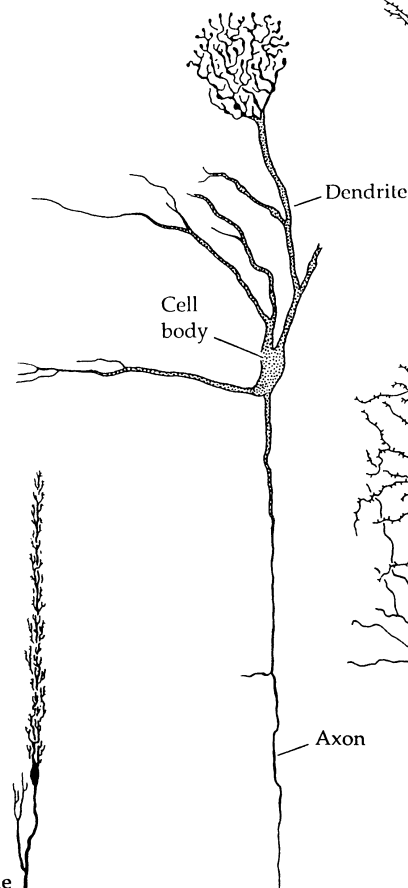


# The Squid Giant Axon...

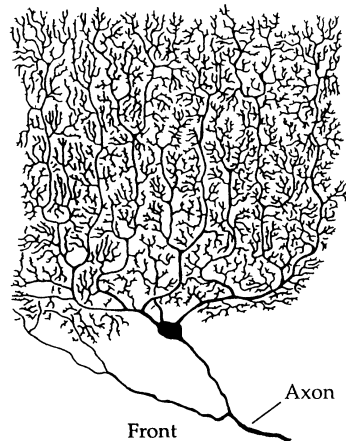
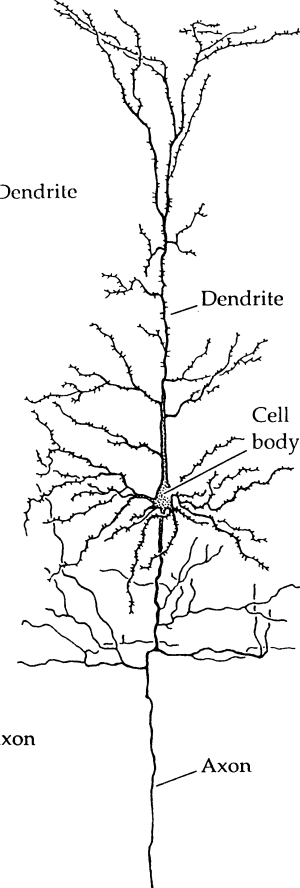
MOTOR NEURON  
FROM SPINAL CORD



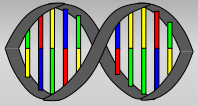
MITRAL CELL FROM  
OLFACTORY BULB



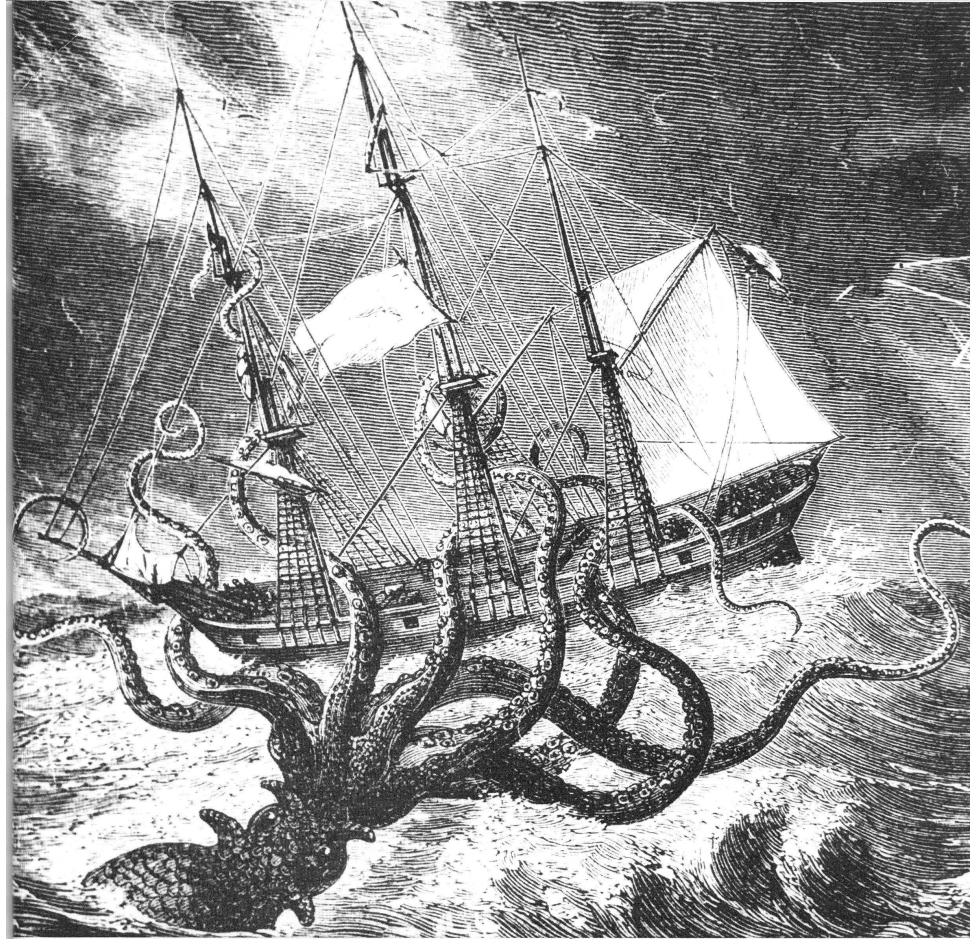
PYRAMIDAL CELL  
FROM CORTEX

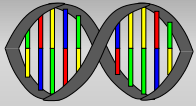


PURKINJE CELL

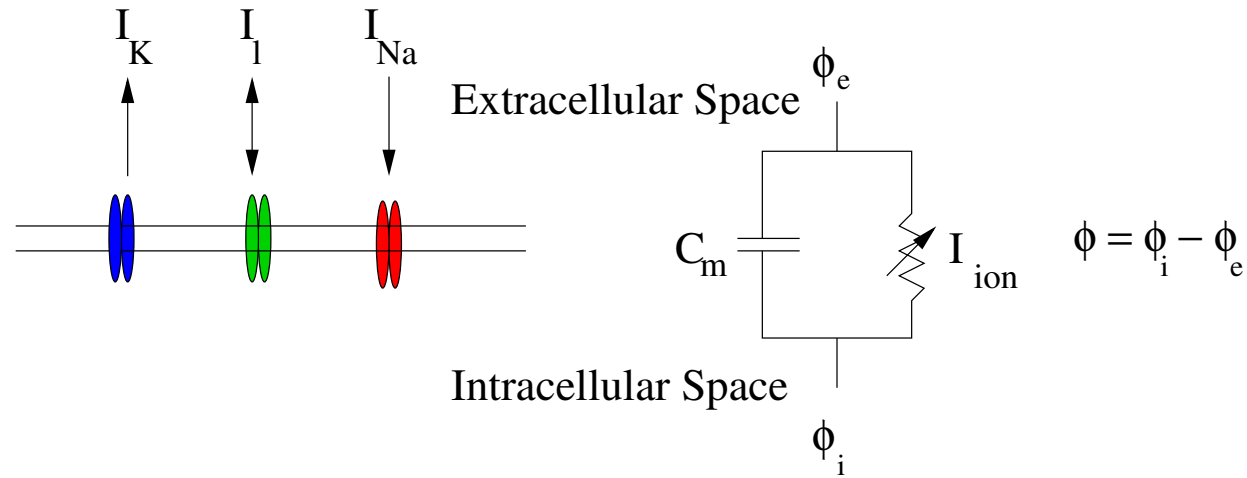


# *is not the Giant Squid Axon*



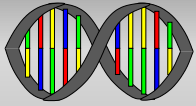


# The Hodgkin-Huxley Equations

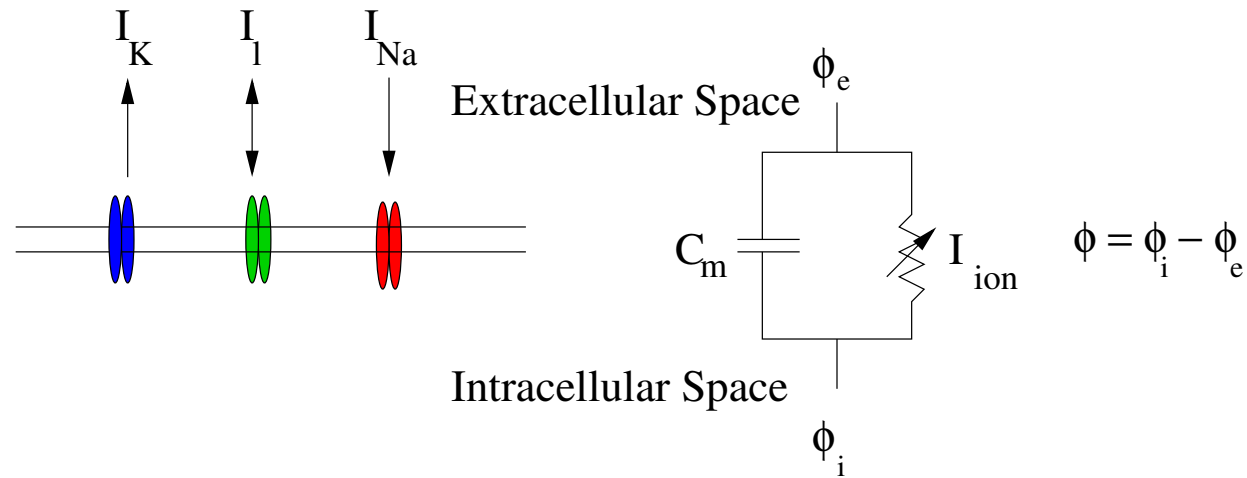


$$C_m \frac{dV}{dt} + I_{Na} + I_K + I_l = 0,$$



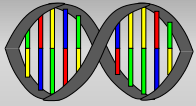


# The Hodgkin-Huxley Equations

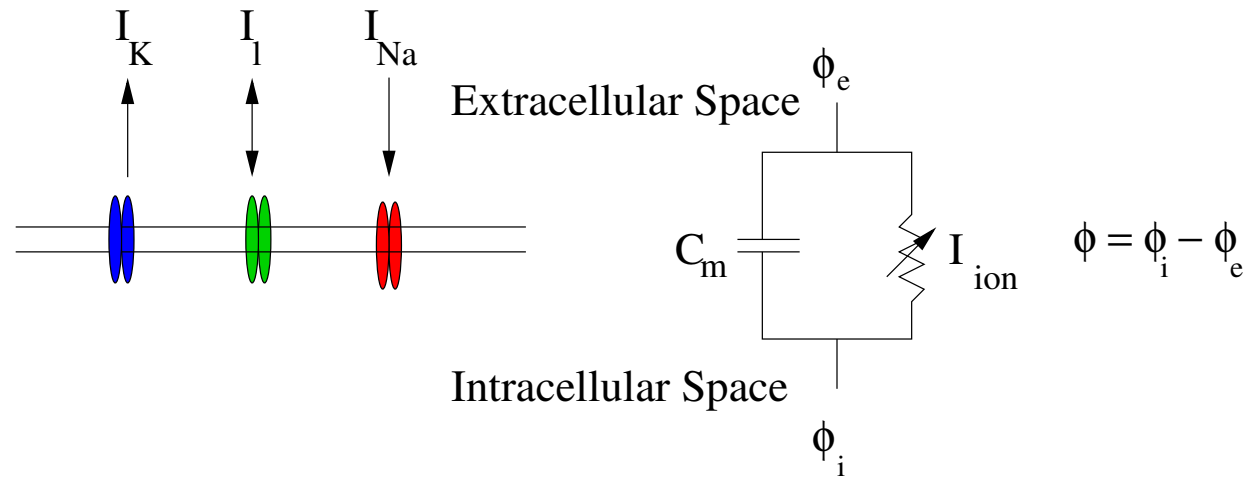


$$C_m \frac{dV}{dt} + \boxed{I_{Na}} + I_K + I_l = 0,$$

with sodium current  $I_{Na}$ ,

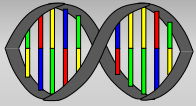


# The Hodgkin-Huxley Equations

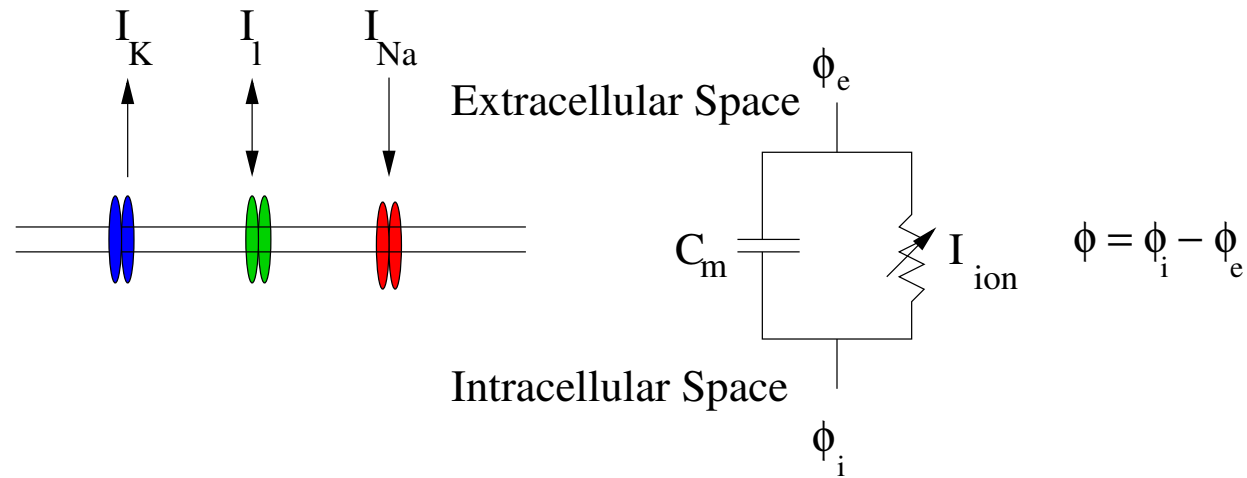


$$C_m \frac{dV}{dt} + \boxed{I_{Na}} + \boxed{I_K} + I_l = 0,$$

with **sodium current**  $I_{Na}$ , **potassium current**  $I_K$ ,

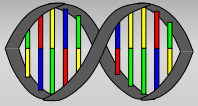


# The Hodgkin-Huxley Equations



$$C_m \frac{dV}{dt} + I_{Na} + I_K + I_l = 0,$$

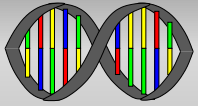
with sodium current  $I_{Na}$ , potassium current  $I_K$ , and leak current  $I_l$ .



# ***Ionic Currents***

Ionic currents are typically of the form

$$I = g(\phi, t) \Phi(\phi)$$

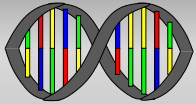


# ***Ionic Currents***

Ionic currents are typically of the form

$$I = \boxed{g(\phi, t)} \Phi(\phi)$$

where  $g(\phi, t)$  is the total number of open channels,

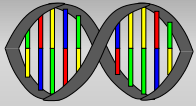


# ***Ionic Currents***

Ionic currents are typically of the form

$$I = g(\phi, t) \Phi(\phi)$$

where  $g(\phi, t)$  is the total number of open channels, and  $\Phi(\phi)$  is the  $I$ - $\phi$  relationship for a single channel.



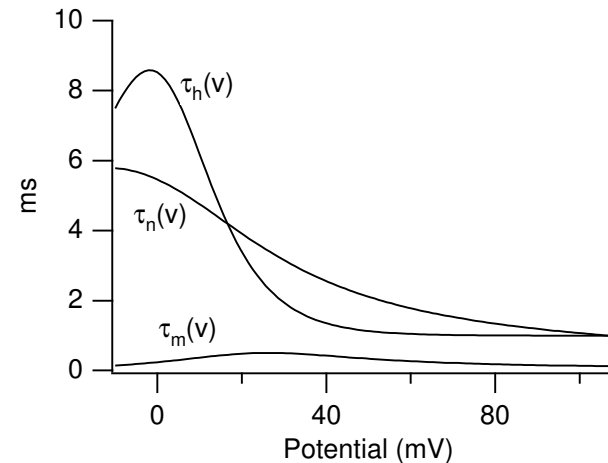
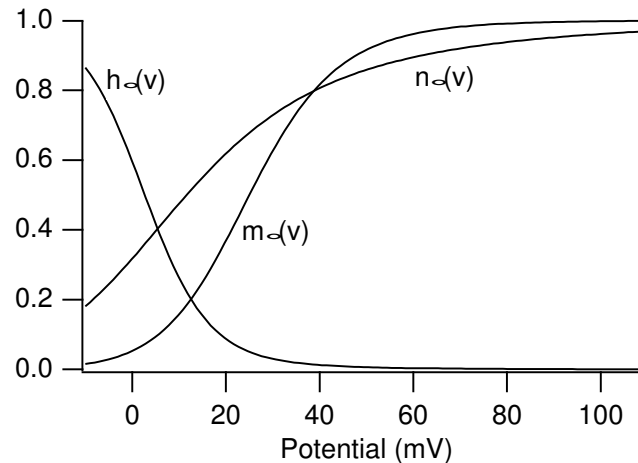
# Currents

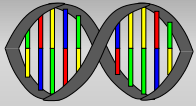
Hodgkin and Huxley found that

$$I_k = g_k n^4 (\phi - \phi_K), \quad I_{Na} = g_{Na} m^3 h (\phi - \phi_{Na}),$$

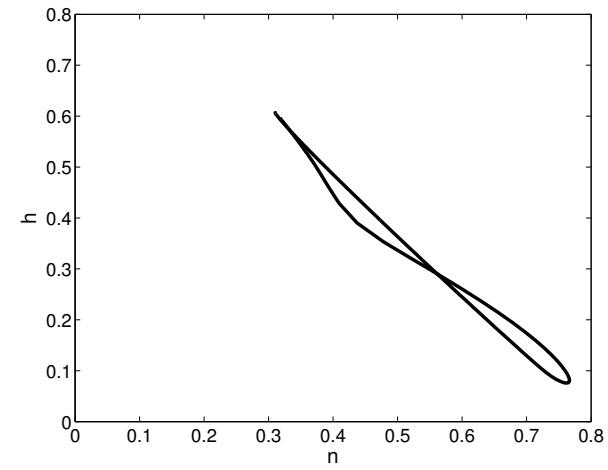
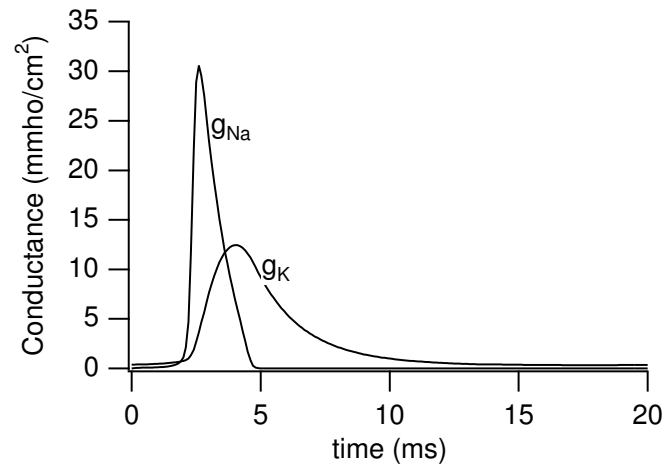
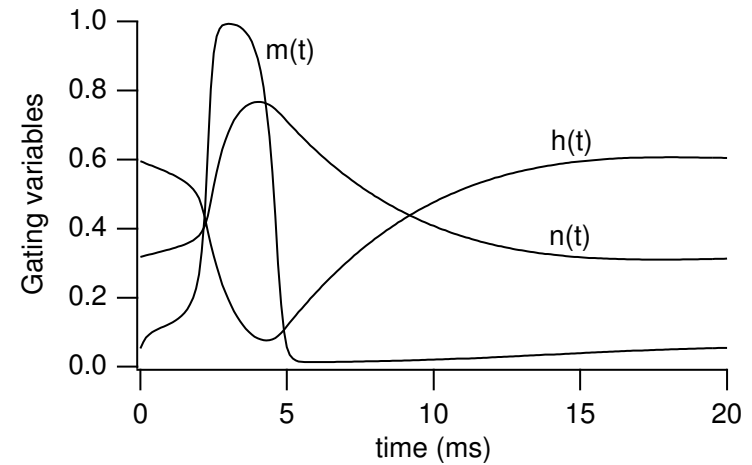
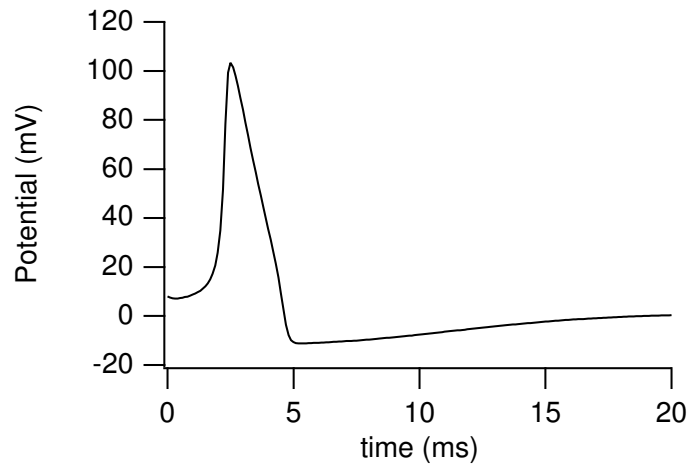
where

$$\tau_u(\phi) \frac{du}{dt} = u_\infty(\phi) - u, \quad u = m, n, h$$

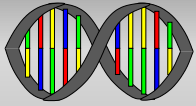




# Action Potential Dynamics

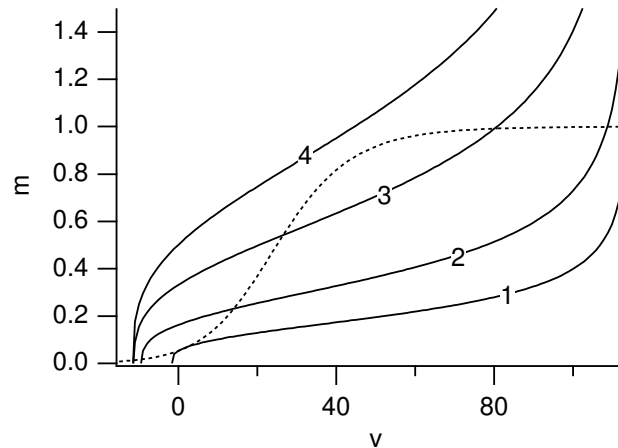
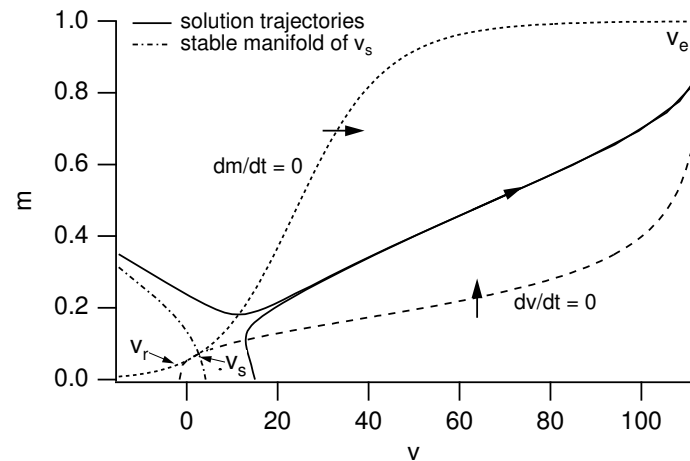


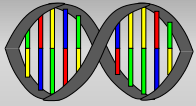




# Fast-Slow Subsystem Dynamics

Observe that  $\tau_m \ll \tau_n, \tau_h$



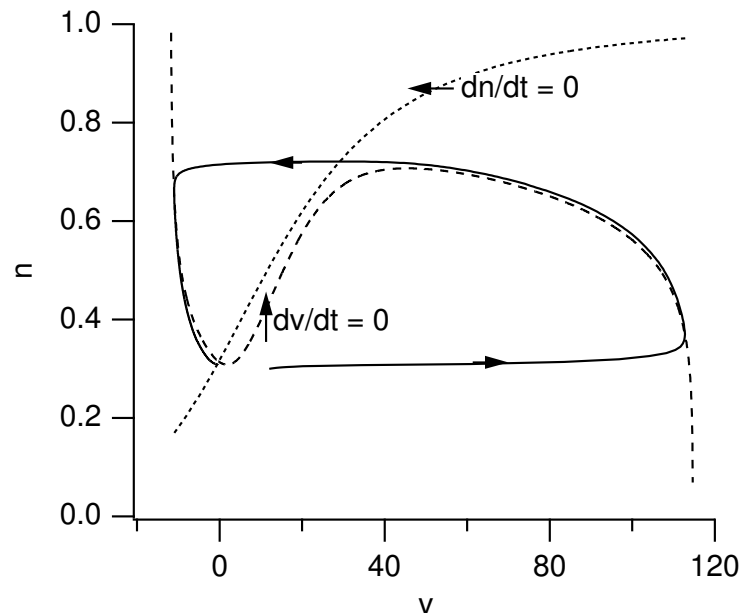


# Two Variable Reduction of HH Eqns

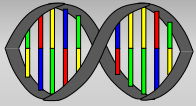
Set  $m = m_\infty(\phi)$ , and set  $h + n \approx N = 0.85$ .  
This reduces to a two variable system

$$C \frac{d\phi}{dt} = \bar{g}_K n^4 (\phi - \phi_K) + \bar{g}_{Na} m_\infty^3(\phi) (N - n) (\phi - \phi_{Na}) + \bar{g}_l (\phi - \phi_L),$$

$$\tau_n(\phi) \frac{dn}{dt} = n_\infty(\phi) - n.$$



(Go Back)



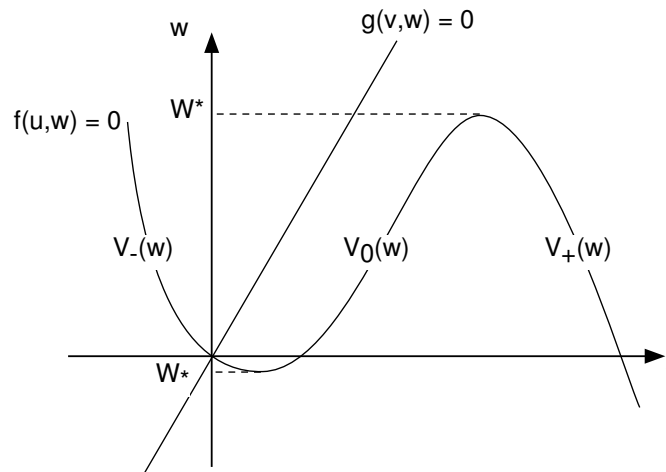
# Two Variable Models

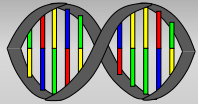
Following is a summary of two variable models of excitable media. The models described here are all of the form

$$\frac{dv}{dt} = f(v, w) + I$$

$$\frac{dw}{dt} = g(v, w)$$

Typically,  $v$  is a “fast” variable, while  $w$  is a “slow” variable.





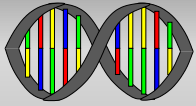
# *Cubic FitzHugh-Nagumo*

The model that started the whole business uses a cubic polynomial (a variant of the van der Pol equation).

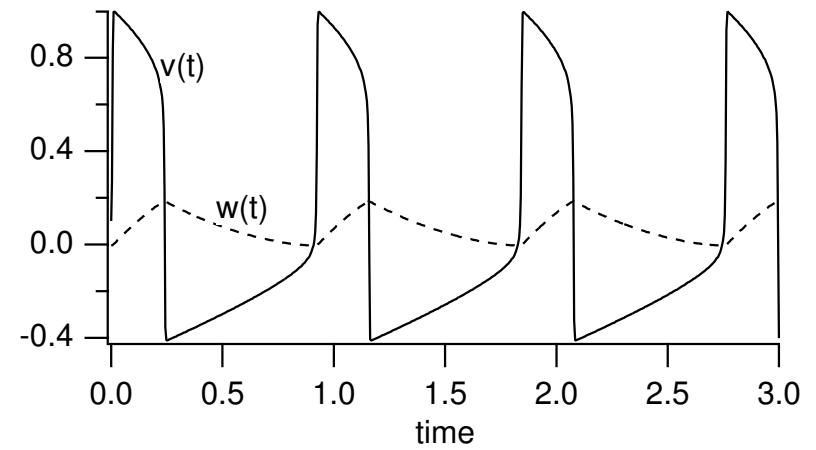
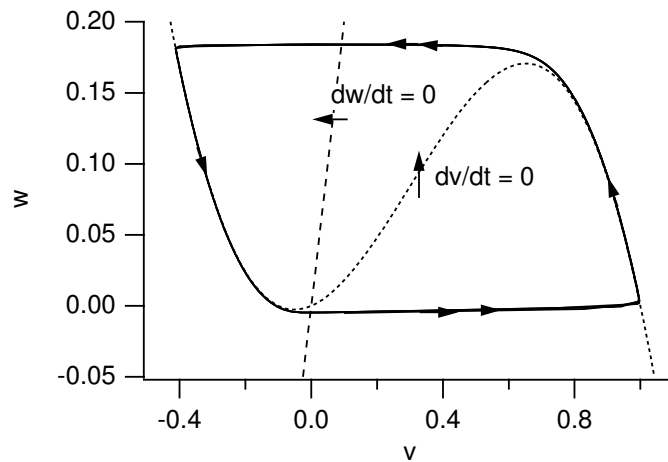
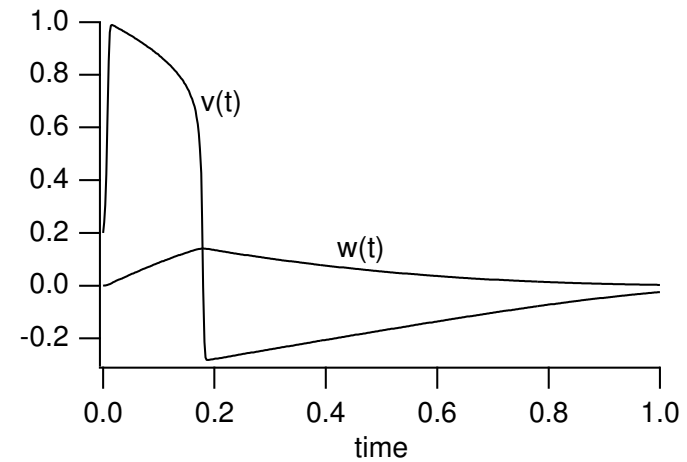
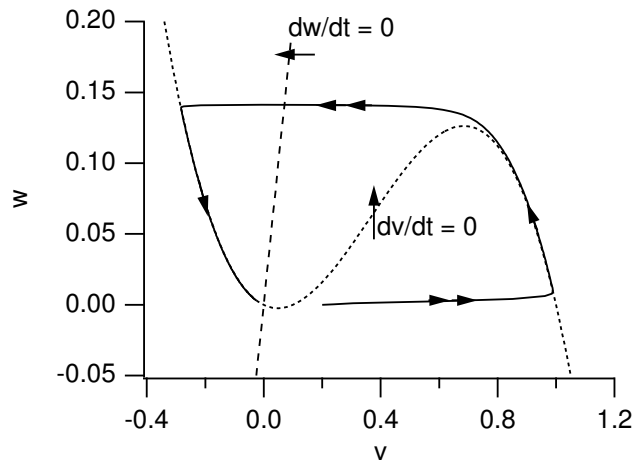
$$F(v, w) = Av(v - \alpha)(1 - v) - w,$$

$$G(v, w) = \epsilon(v - \gamma w).$$

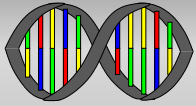
with  $0 < \alpha < \frac{1}{2}$ , and  $\epsilon$  “small”.



# FitzHugh-Nagumo Equations



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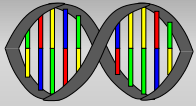


Mitchell-Schaeffer two-variable model (also in a slightly different but equivalent form by Karma)

$$F(v, w) = \frac{1}{\tau_{in}} w v^2 (1 - v) - \frac{v}{\tau_{out}},$$

$$G(v, w) = \begin{cases} \frac{1}{\tau_{open}} (1 - w) & v < v_{gate} \\ -\frac{w}{\tau_{close}} & v > v_{gate} \end{cases}$$

Notice that  $F(v, w)$  is cubic in  $v$ , and  $w$  is an inactivation variable (like  $h$  in HH).



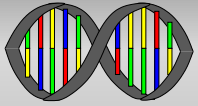
# Mitchell-Schaeffer Revised

To make the Mitchell-Schaeffer look like an ionic model, take

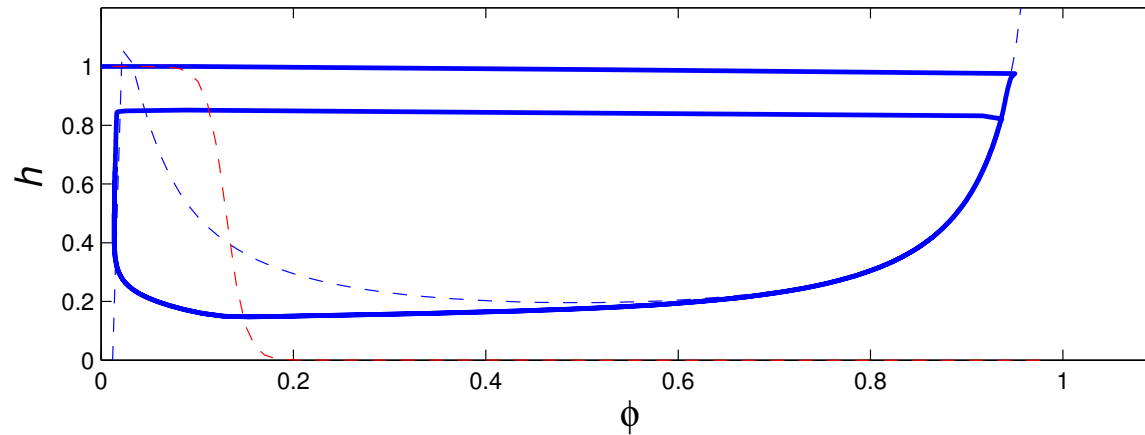
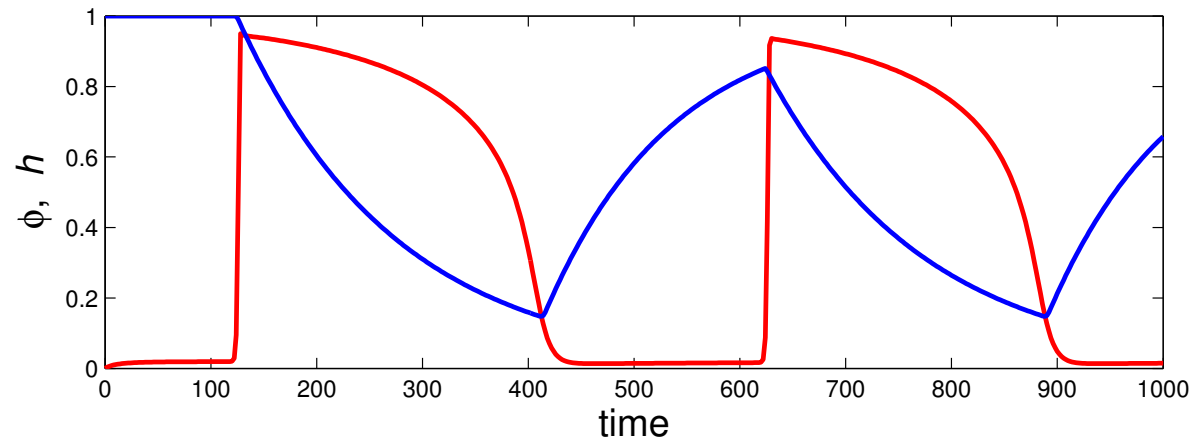
$$\begin{aligned} C_m \frac{dv}{dt} &= g_{Na} h m^2 (V_{Na} - v) + g_K (V_K - v), \\ \tau_h \frac{dh}{dt} &= h_\infty(v) - h \end{aligned}$$

where

$$m(v) = \begin{cases} 0, & v < 0 \\ v, & 0 < v < 1 \\ 1, & v > 1 \end{cases}, \quad \begin{aligned} h_\infty &= 1 - f(v), \\ \tau_h &= \tau_{open} + (\tau_{close} - \tau_{open}) f(v) \\ f(v) &= \frac{1}{2} (1 + \tanh(\kappa(v - v_{gate}))), \end{aligned}$$

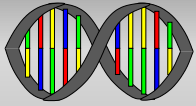


# Mitchell-Schaeffer Revised-II



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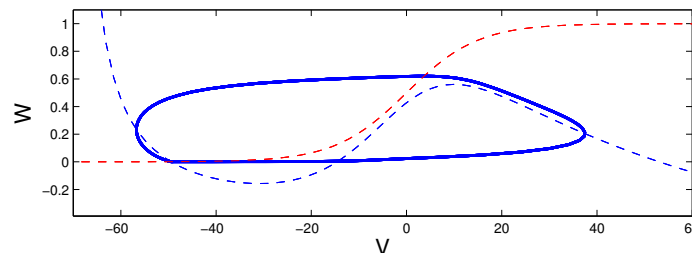
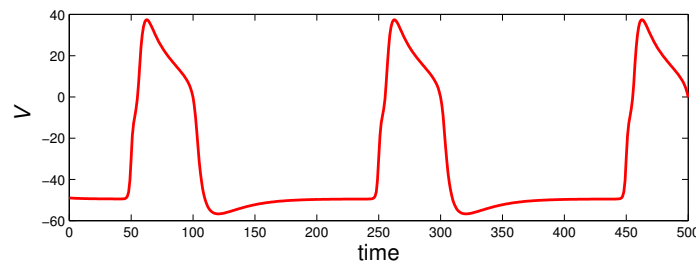
# Morris-Lecar

This model was devised for barnacle muscle fiber.

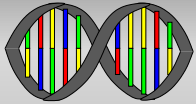
$$F(v, w) = -g_{ca}m_{\infty}(v)(v - v_{ca}) - g_k w(v - v_k) - g_l(v - v_l) + I_{app}$$

$$G(v, w) = \phi \cosh\left(\frac{1}{2} \frac{v - v_3}{v_4}\right)(w_{\infty}(v) - w),$$

$$m_{\infty}(v) = \frac{1}{2} + \frac{1}{2} \tanh\left(\frac{v - v_1}{v_2}\right), \quad w_{\infty}(v) = \left(1 + \tanh\left(\frac{v - v_3}{2v_4}\right)\right).$$

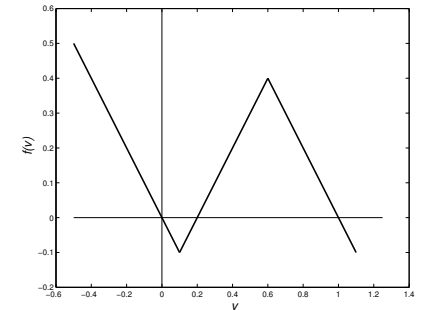


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McKean suggested two piecewise linear models with  $F(v, w) = f(v) - w$  and  $G(v, w) = \epsilon(v - \gamma w)$ . For the first,

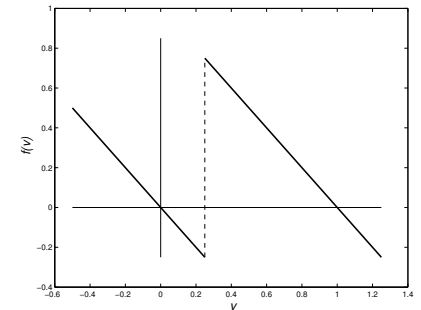
$$f(v) = \begin{cases} -v & v < \frac{\alpha}{2} \\ v - \alpha & \frac{\alpha}{2} < v < \frac{1+\alpha}{2} \\ 1 - v & v > \frac{1+\alpha}{2} \end{cases}$$



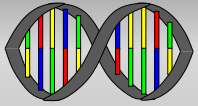
where  $0 < \alpha < \frac{1}{2}$ .

The second model suggested by McKean had

$$f(v) = \begin{cases} -v & v < \alpha \\ 1 - v & v > \alpha \end{cases}$$



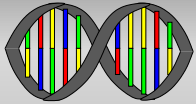
and  $\gamma = 0$ .



A model devised to give very fast 2D computations (the code is known as EZspiral)

$$F(v, w) = v(1 - v)\left(v - \frac{w + b}{a}\right),$$

$$G(v, w) = \epsilon(v - w).$$



A piecewise linear model devised to match cardiac restitution properties

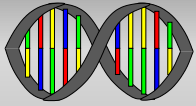
$$F(v, w) = f(v) - w$$

$$G(v, w) \frac{1}{\tau(v)} (v - w)$$

where

$$f(v) = \begin{cases} -30v, & v < v_1 \\ \gamma v - 0.12, & v_1 < v < v_2, \\ -30(v - 1), & v > v_2 \end{cases}, \quad \tau(v) = \begin{cases} 2 & v < \\ 16.6 & v > \end{cases}$$

with  $v_1 = \frac{0.12}{30+\gamma}$ ,  $v_2 = \frac{30.12}{30+\gamma}$ . (Go Back)



For the Aliev model,

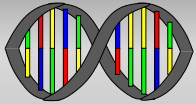
$$F(v, w) = g_a(v - \beta)(v - \alpha)(1 - v) - vw$$

$$G(v, w) = -\epsilon(v, w)(w + g_s(v - \beta)(v - \alpha - 1))$$

where  $\epsilon(v, w) = \epsilon_1 + \mu_1 \frac{w}{v + \mu_2}$ .

Reasonable parameter values are  $\beta = 0.0001$ ,  $\alpha = 0.05$ ,  $g_a = 8.0$ ,

$g_s = 8.0$ ,  $\mu_1 = 0.05$ ,  $\mu_2 = 0.3$ ,  $\epsilon_1 = 0.03$ ,  $\epsilon_2 = 0.0001$ .

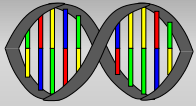


These dynamics describe the oxidation-reduction of malonic acid. For this system,

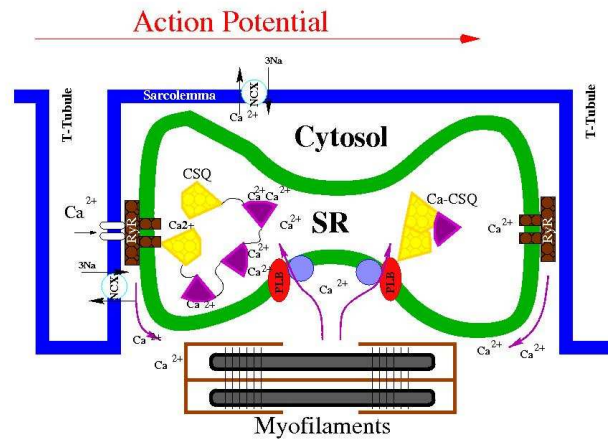
$$F(v, w) = v - v^2 - (fw + \phi_0) \frac{v - q}{v + q} \quad (-10)$$

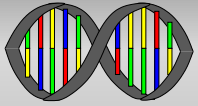
$$G(v, w) = \epsilon(v - w) \quad (-10)$$

with typical parameter values  $\epsilon = 0.05$ ,  $q = 0.002$ ,  $f = 3.5$ ,  $\phi_0 = 0.01$ .



# Intracellular Calcium





# ***Features of Excitable Systems***

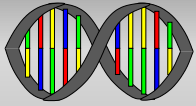
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Threshold Behavior, Refractoriness

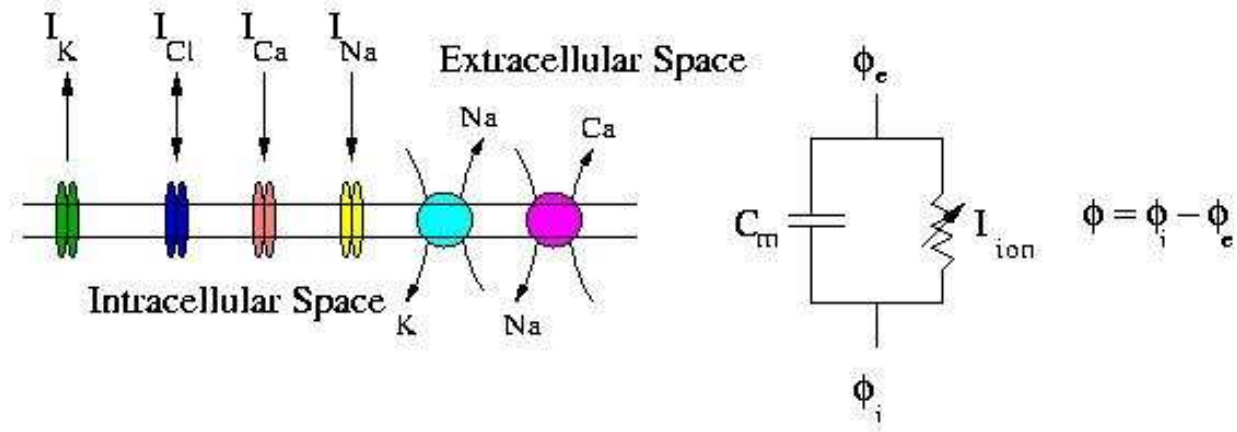
Alternans

Wenckebach Patterns





# Cardiac Models



All cardiac models are of the form

$$C_m \frac{d\phi}{dt} + I_{ion}(\phi, w, [Ion]) = I_{in}$$

with currents, gating and concentrations for sodium, potassium, calcium, and chloride ions.