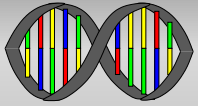


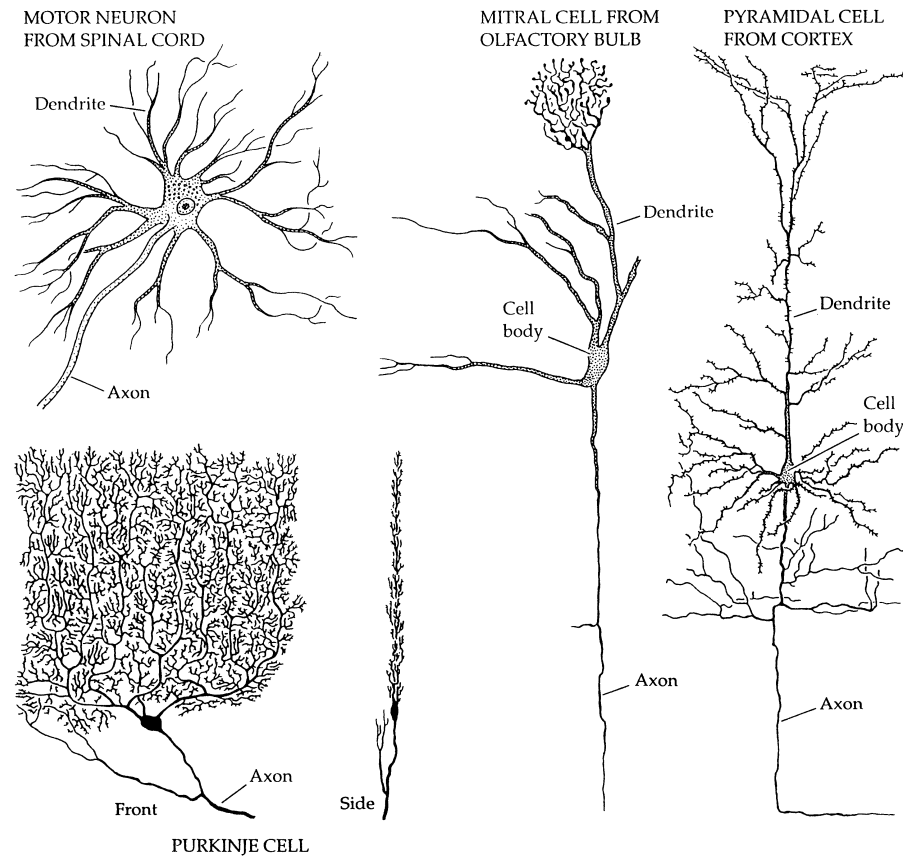
# ***Coupling and Propagation in Excitable Media***

J. P. Keener

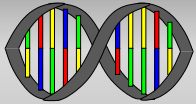
Mathematics Department  
University of Utah



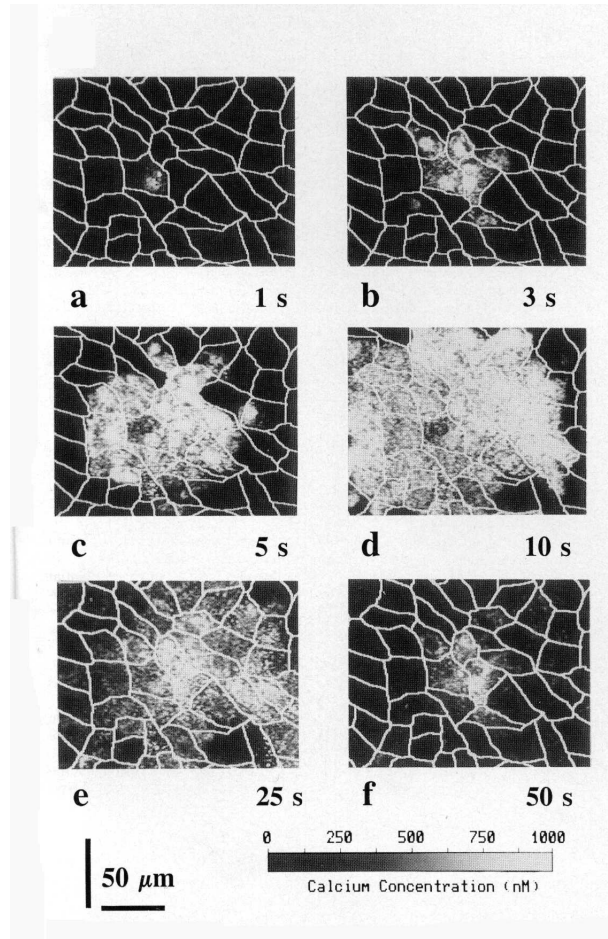
# ***Spatially Extended Excitable Media***



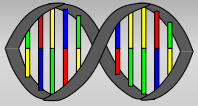
## Neurons and axons



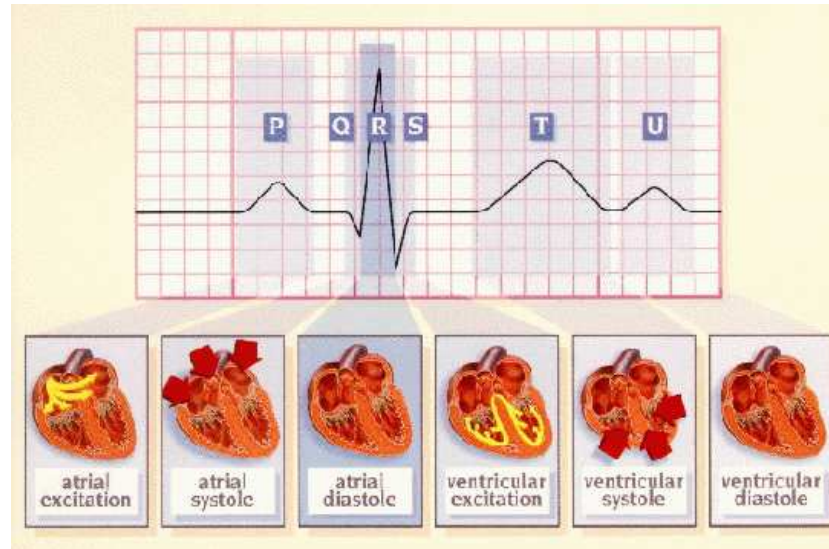
# *Spatially Extended Excitable Media*

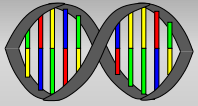


Mechanically stimulated Calcium waves

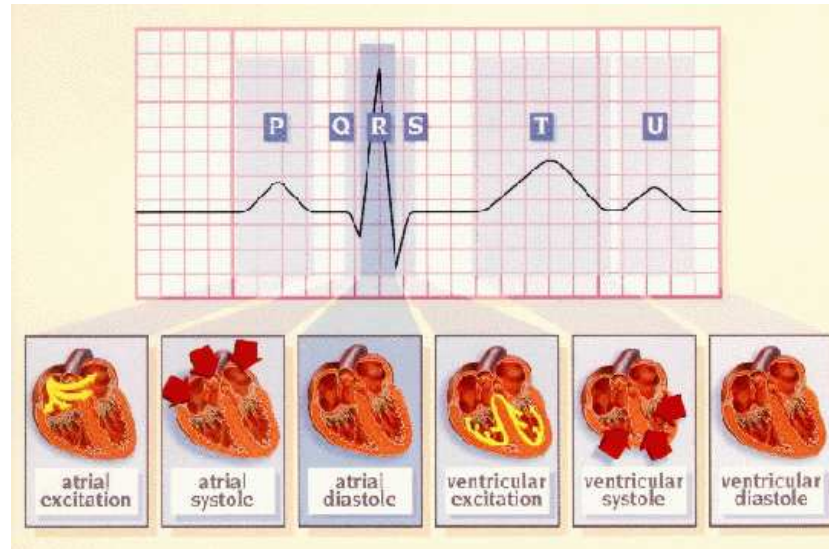


# *Conduction system of the heart*

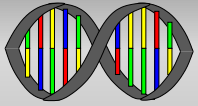




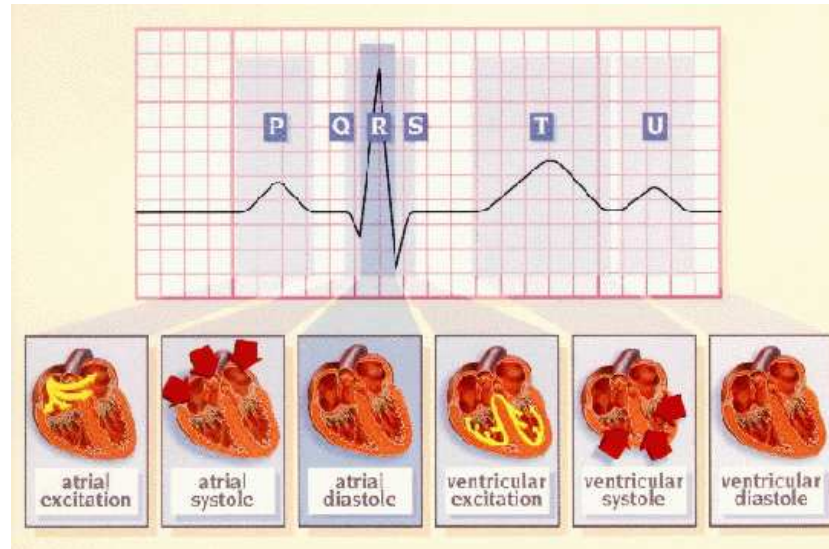
# *Conduction system of the heart*



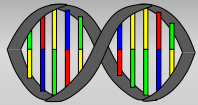
- Electrical signal originates in the SA node.



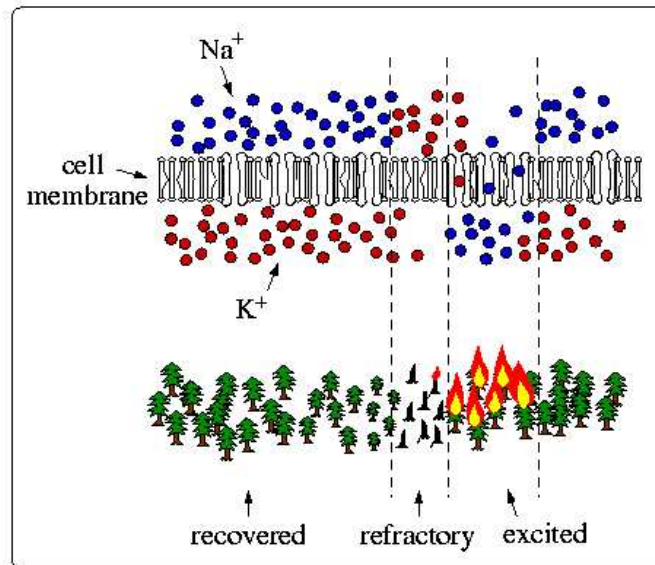
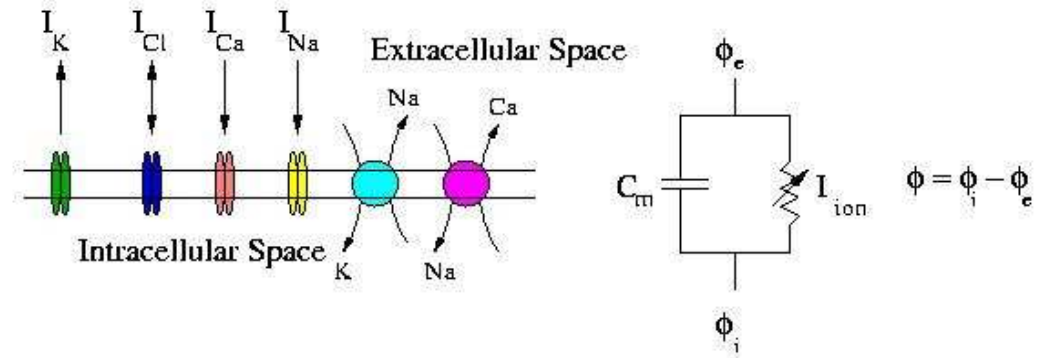
# *Conduction system of the heart*



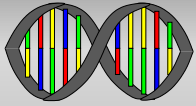
- Electrical signal originates in the SA node.
- The signal propagates across the atria (2D sheet), through the AV node, along Purkinje fibers (1D cables), and throughout the ventricles (3D tissue).



# Spatially Extended Excitable Media



The forest fire analogy



# Spatial Coupling

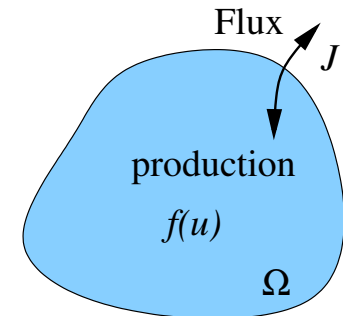
Conservation Law:

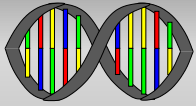
$$\frac{d}{dt}(\text{stuff in } \Omega) = \text{rate of transport} + \text{rate of production}$$

$$\frac{d}{dt} \int_{\Omega} u dV = \int_{\partial\Omega} J \cdot n ds + \int_{\Omega} f dv$$

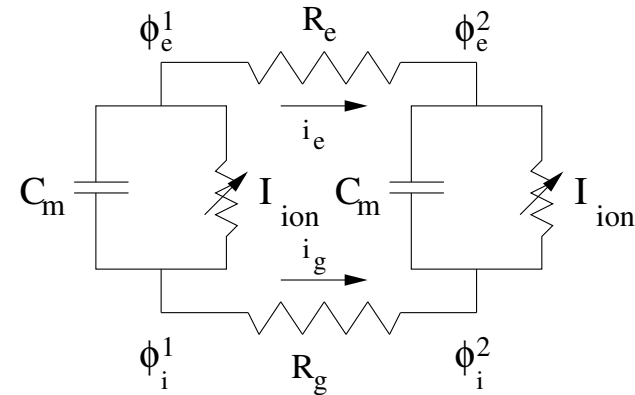
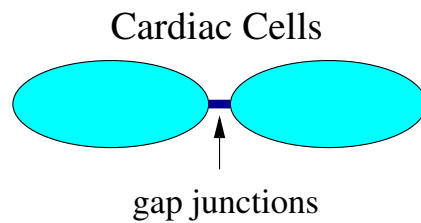
becomes

$$\frac{\partial u}{\partial t} = \nabla \cdot (D \nabla u) + f(u)$$





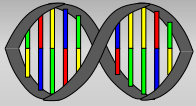
# Coupled Cells



$$C_m \frac{d\phi^1}{dt} + I_{ion}(\phi^1, w) = -i_i = \frac{1}{R_e + R_g} (\phi^2 - \phi^1)$$

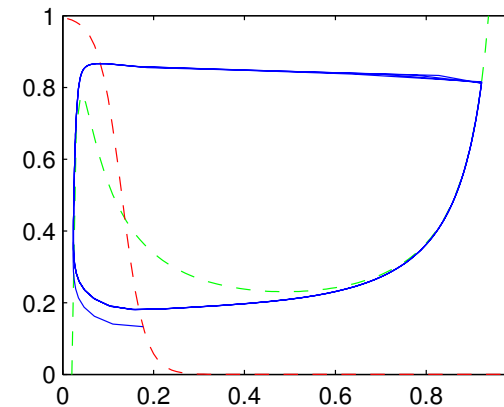
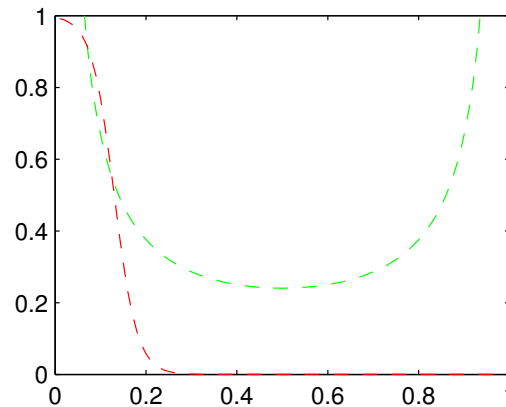
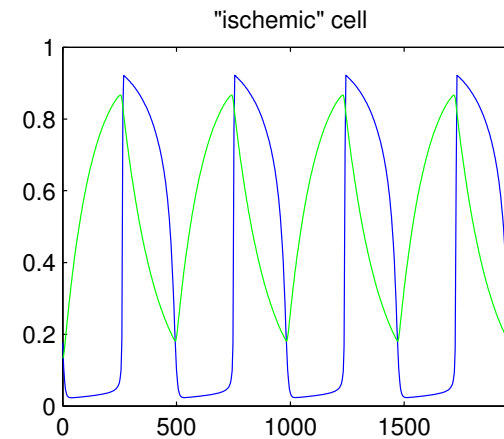
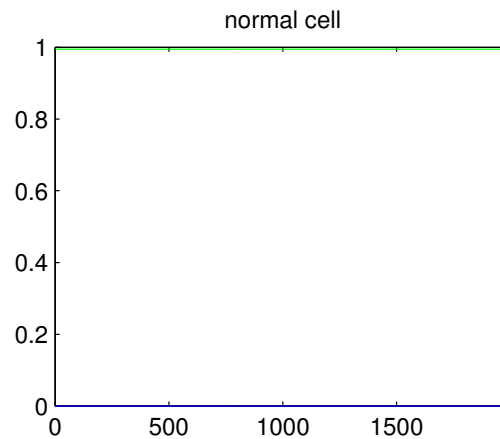
$$C_m \frac{d\phi^2}{dt} + I_{ion}(\phi^2, w) = i_i = \frac{1}{R_e + R_g} (\phi^1 - \phi^2)$$

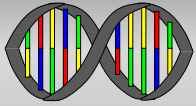
Question: Can anything interesting happen with coupled cells that does not happen with a single cell?



# Coupled Cells

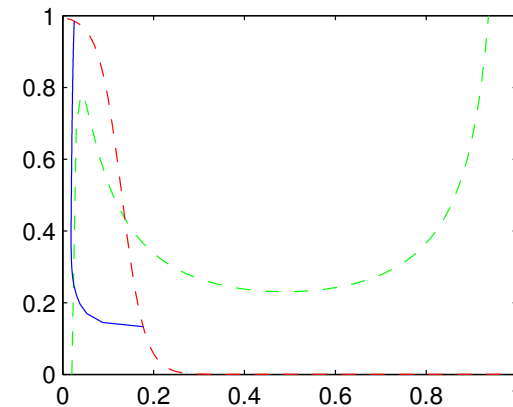
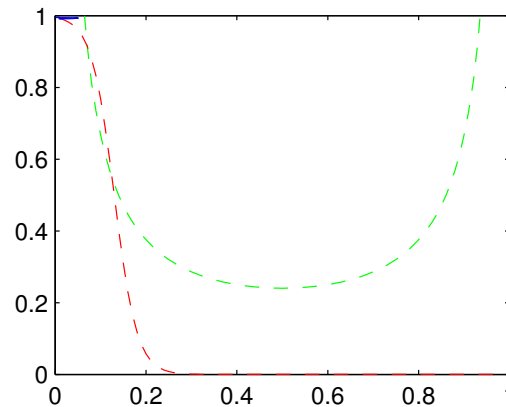
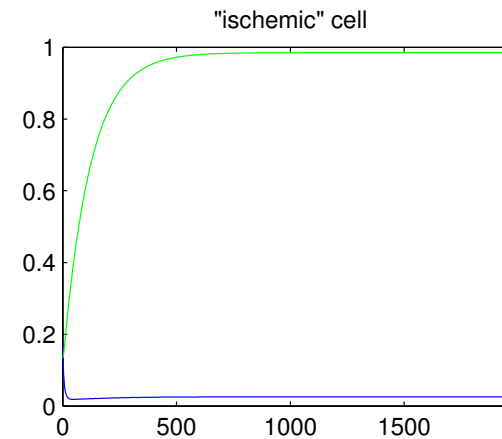
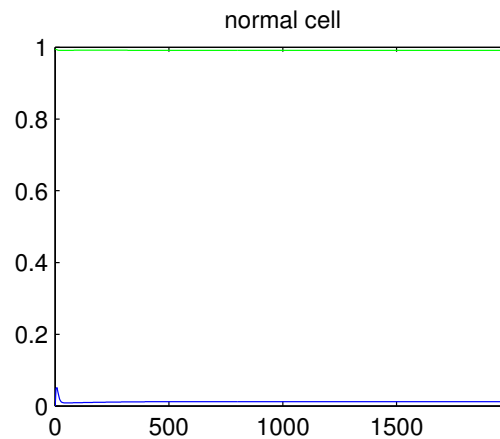
Normal cell and cell with slightly elevated potassium - uncoupled

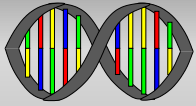




# Coupled Cells

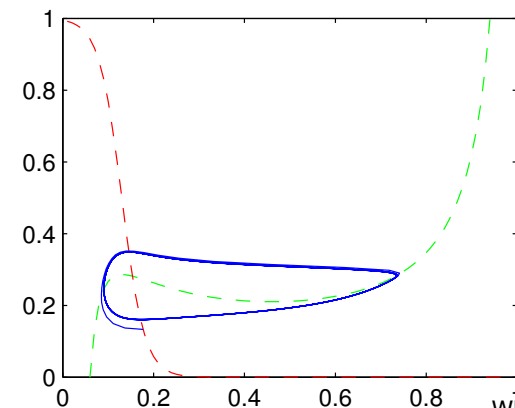
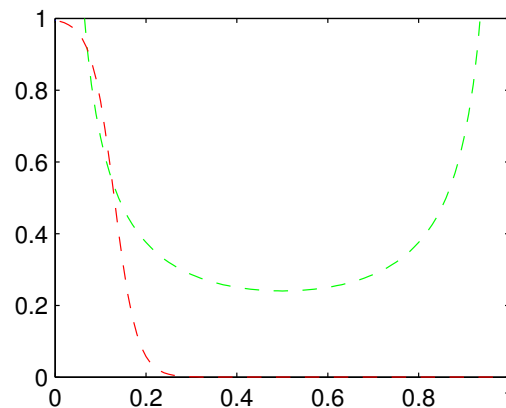
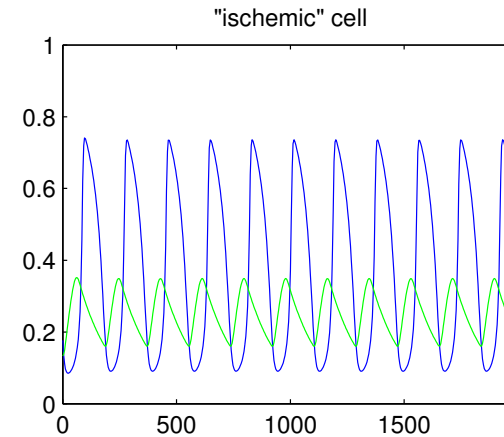
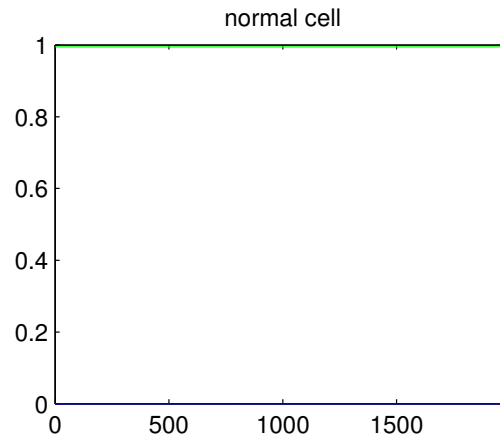
Normal cell and cell with slightly elevated potassium - **coupled**

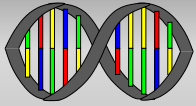




# Coupled Cells

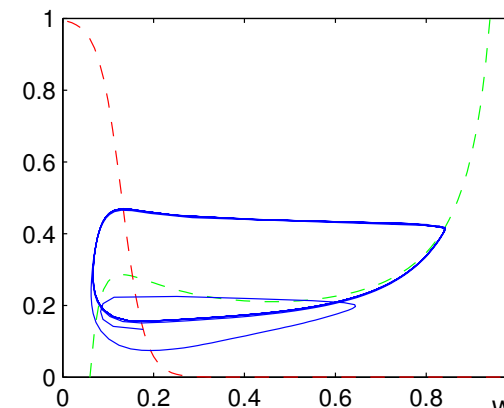
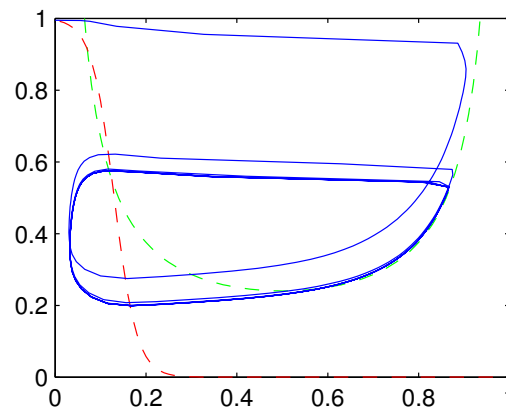
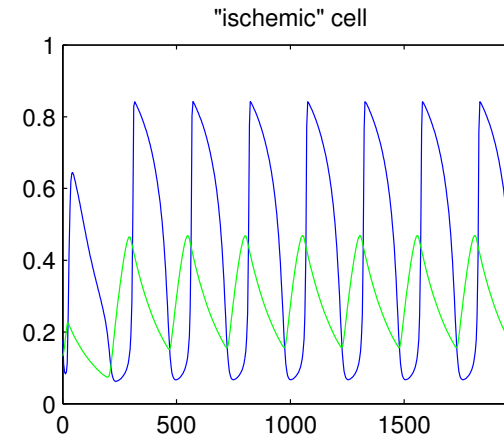
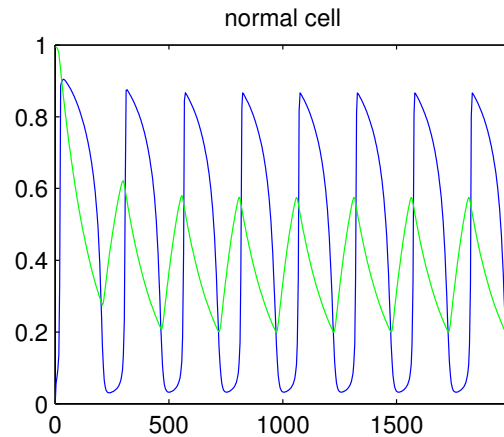
Normal cell and cell with moderately elevated potassium - uncoupled



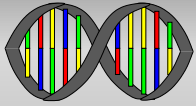


# Coupled Cells

Normal cell and cell with moderately elevated potassium -  
**coupled**

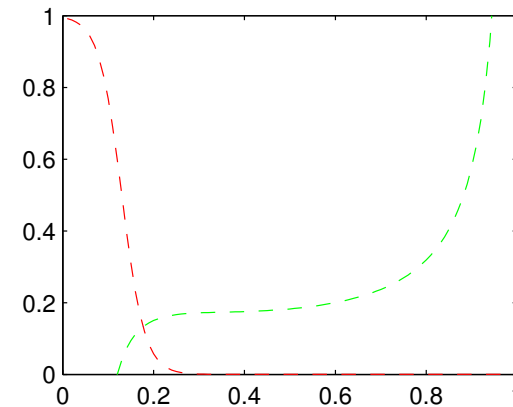
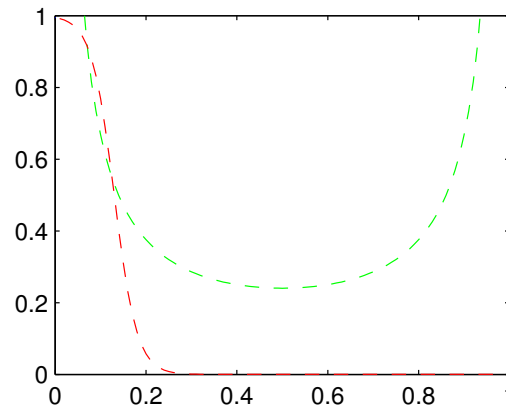
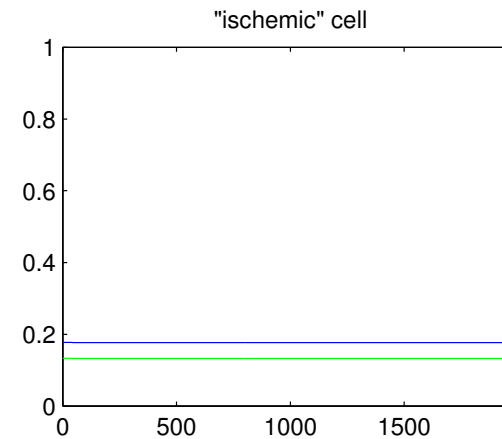
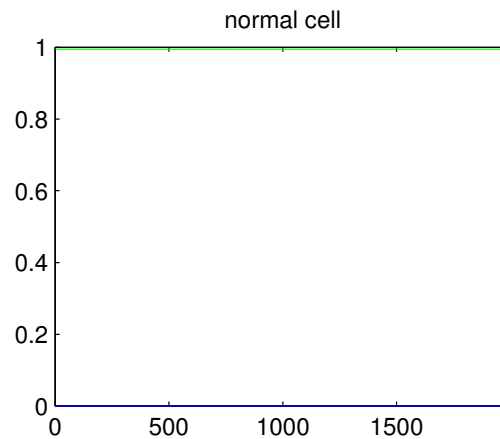


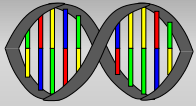
Who could have guessed? – p.8/22



# Coupled Cells

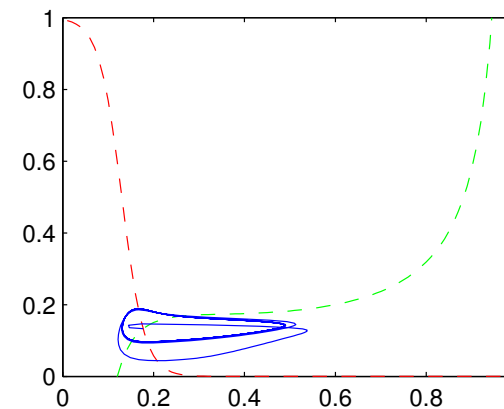
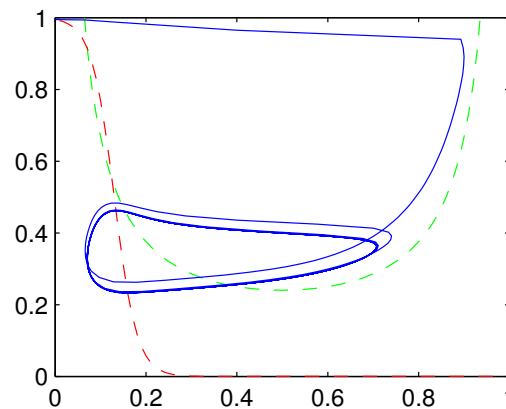
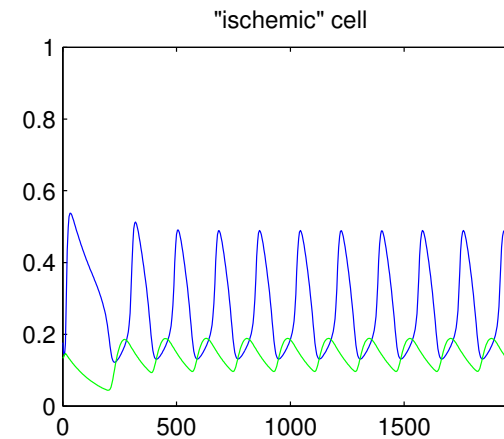
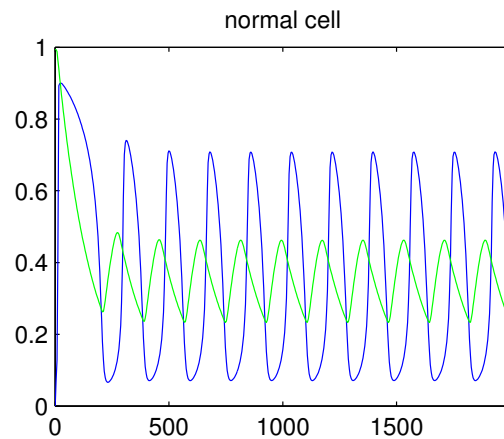
Normal cell and cell with greatly elevated potassium - uncoupled

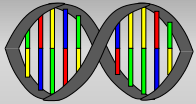




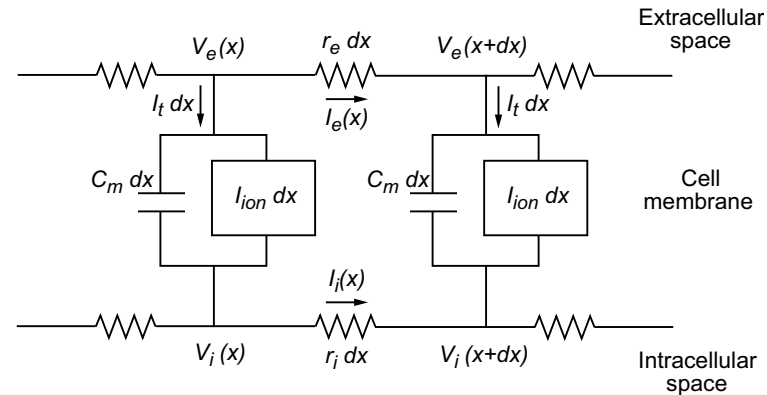
# Coupled Cells

Normal cell and cell with greatly elevated potassium - **coupled**





# Axons and Fibers

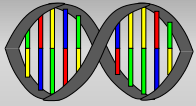


From Ohm's law

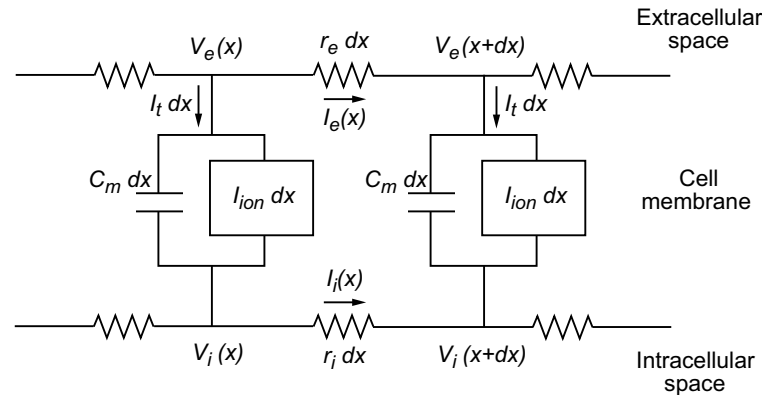
$$V_i(x+dx) - V_i(x) = -I_i(x)r_i dx, \quad V_e(x+dx) - V_e(x) = -I_e(x)r_e dx,$$

In the limit as  $dx \rightarrow 0$ ,

$$I_i = -\frac{1}{r_i} \frac{dV_i}{dx}, \quad I_e = -\frac{1}{r_e} \frac{dV_e}{dx}.$$



# The Cable Equation

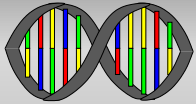


From Kirchhoff's laws

$$I_i(x) - I_i(x + dx) = I_t dx = I_e(x + dx) - I_e(x)$$

In the limit as  $dx \rightarrow 0$ , this becomes

$$I_t = -\frac{\partial I_i}{\partial x} = \frac{\partial I_e}{\partial x}.$$



# ***The Cable Equation***

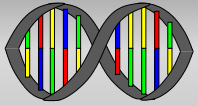
Combining these

$$I_t = \frac{\partial}{\partial x} \left( \frac{1}{r_i + r_e} \frac{\partial V}{\partial x} \right),$$

and, thus,

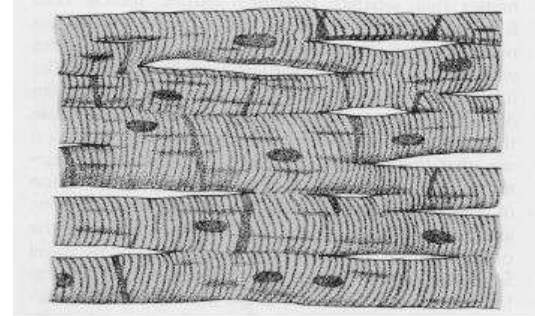
$$C_m \frac{\partial V}{\partial t} + I_{ion} = I_t = \frac{\partial}{\partial x} \left( \frac{1}{r_i + r_e} \frac{\partial V}{\partial x} \right).$$

This equation is referred to as the **cable equation**.

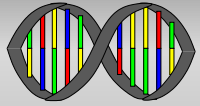


# Modelling Cardiac Tissue

## Cardiac Tissue - The Bidomain Model:

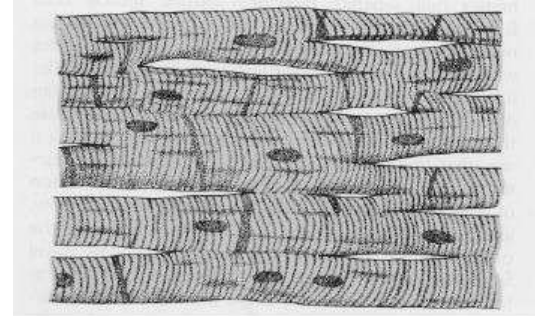


- At each point of the cardiac domain there are two comingled regions, the **extracellular** and the **intracellular** domains with potentials  $\phi_e$  and  $\phi_i$ , and **transmembrane potential**  
$$\phi = \phi_i - \phi_e.$$

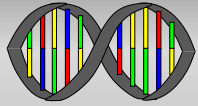


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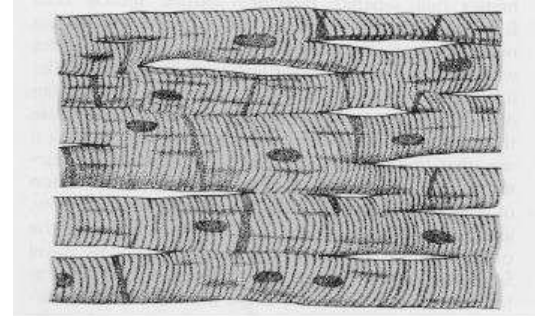


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- These potentials drive currents,  $i_e = -\sigma_e \nabla \phi_e$ ,  $i_i = -\sigma_i \nabla \phi_i$ , where  $\sigma_e$  and  $\sigma_i$  are **conductivity tensors**.



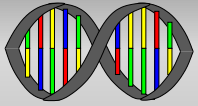
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## Cardiac Tissue - The Bidomain Model:



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- Total current is*

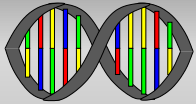
$$i_T = i_e + i_i = -\sigma_e \nabla \phi_e - \sigma_i \nabla \phi_i.$$



## ***Kirchhoff's laws:***

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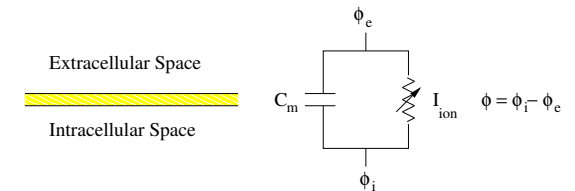
- Total current is conserved:  $\nabla \cdot (\sigma_i \nabla \phi_i + \sigma_e \nabla \phi_e) = 0$

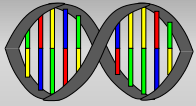


# Kirchhoff's laws:

- Total current is conserved:  $\nabla \cdot (\sigma_i \nabla \phi_i + \sigma_e \nabla \phi_e) = 0$
- Transmembrane current is balanced:

$$\chi \left( C_m \frac{\partial \phi}{\partial \tau} + I_{ion} \right) = \nabla \cdot (\sigma_i \nabla \phi_i)$$

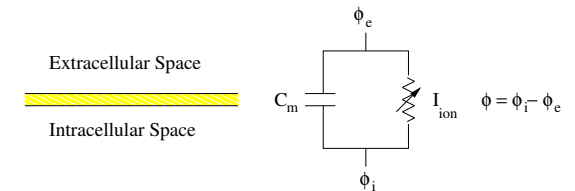




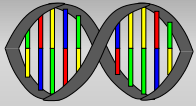
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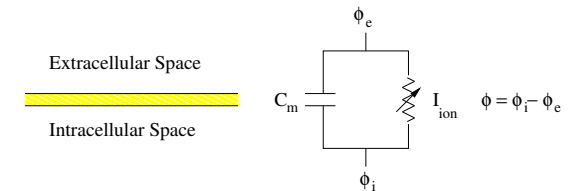
surface to volume ratio,



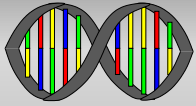
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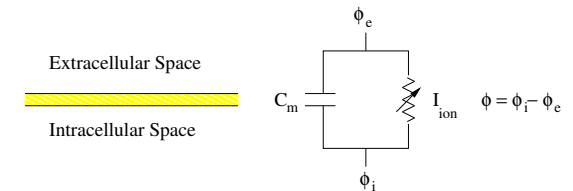
surface to volume ratio, capacitive current,



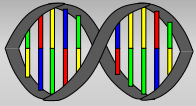
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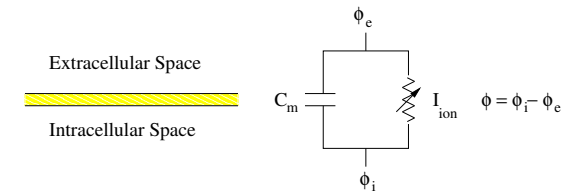
surface to volume ratio, capacitive current, ionic current,



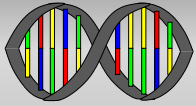
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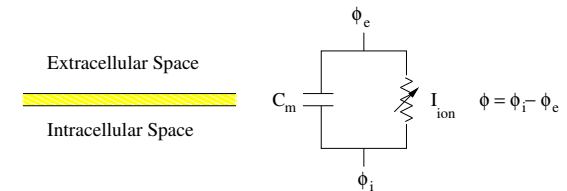
surface to volume ratio, capacitive current, ionic current,  
and current from intracellular space.



# Kirchhoff's laws:

- Total current is conserved:  $\nabla \cdot (\sigma_i \nabla \phi_i + \sigma_e \nabla \phi_e) = 0$
- Transmembrane current is balanced:

$$\chi \left( C_m \frac{\partial \phi}{\partial \tau} + I_{ion} \right) = \nabla \cdot (\sigma_i \nabla \phi_i)$$

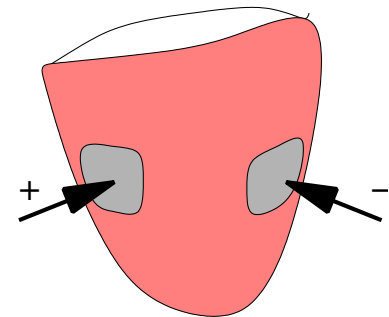


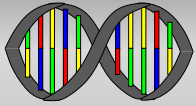
surface to volume ratio, capacitive current, ionic current, and current from intracellular space.

- Boundary conditions:

$$\mathbf{n} \cdot \sigma_i \nabla \phi_i = 0, \quad \mathbf{n} \cdot \sigma_e \nabla \phi_e = I(t, x)$$

and  $\int_{\partial\Omega} I(t, x) dx = 0$  on  $\partial\Omega$ .



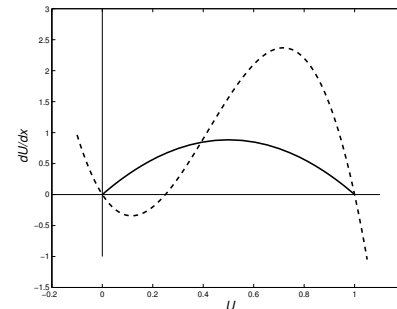
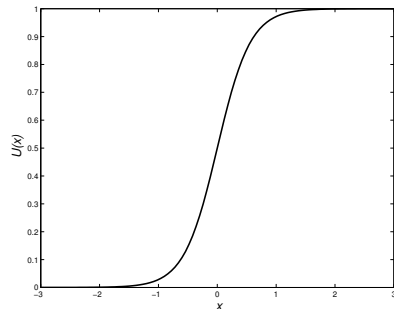


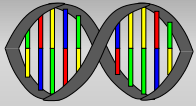
# The Bistable Equation

$$\frac{\partial u}{\partial t} = D \frac{\partial^2 u}{\partial x^2} + f(u)$$

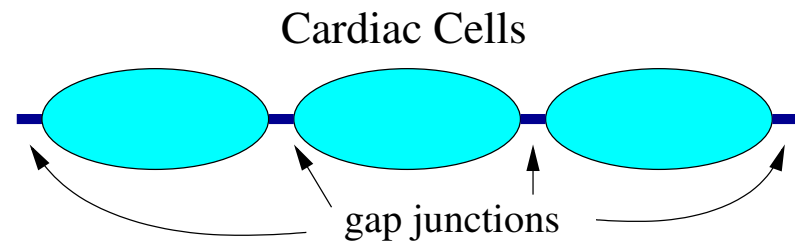
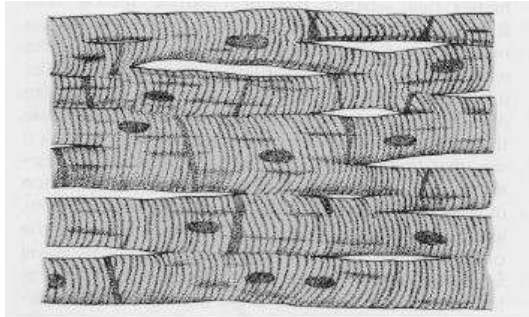
with  $f(0) = f(a) = f(1) = 0$ ,  $0 < a < 1$ .

- There is a unique traveling wave solution  $u = U(x - ct)$ ,
- The solution is stable up to phase shifts,
- The speed scales as  $c = c_0 \sqrt{D}$ ,
- $U$  is a homoclinic trajectory of  $DU'' + cU' + f(U) = 0$

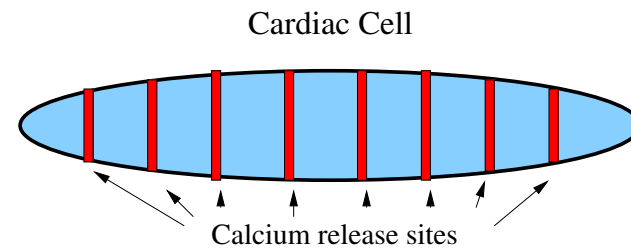
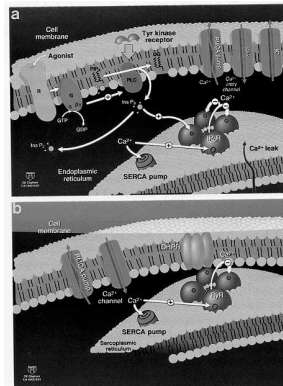




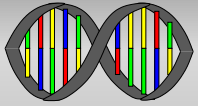
# Discreteness



## Gap junctional coupling



## Calcium Release through CICR Receptors



# ***Discrete Effects***

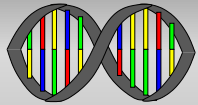
## Discrete Cells

$$\frac{dv_n}{dt} = f(v_n) + d(v_{n-1} - 2v_n + v_{n+1})$$

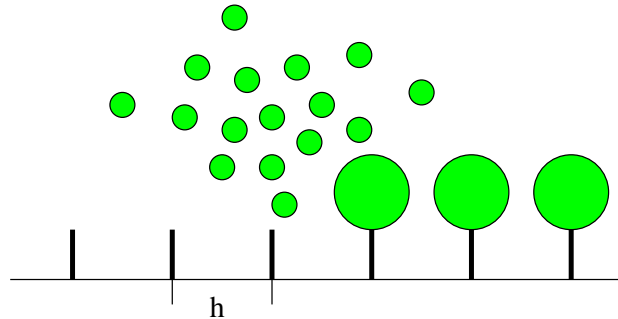
## Discrete Calcium Release

## Discrete Release Sites

$$\frac{\partial u}{\partial t} = D \frac{\partial^2 u}{\partial x^2} + g(x)f(u)$$



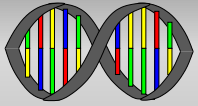
# Fire-Diffuse-Fire Model



Suppose a diffusible chemical  $u$  is released from

- a long line of evenly spaced release sites;
- Release of full contents  $C$  occurs when concentration  $u$  reaches threshold  $\theta$ .

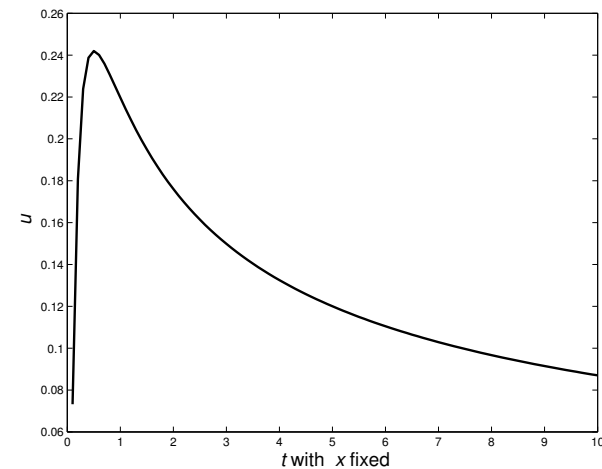
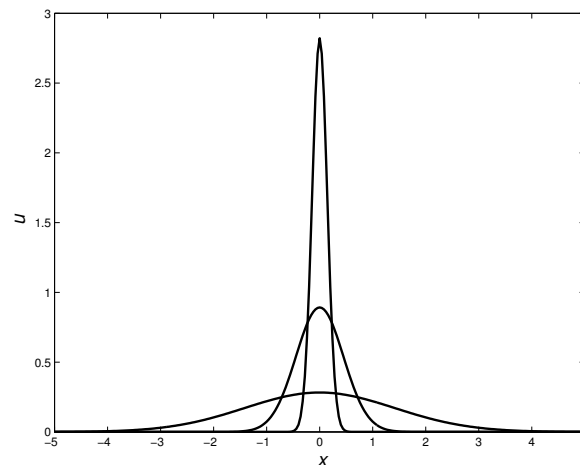
$$\frac{\partial u}{\partial t} = D \frac{\partial^2 u}{\partial x^2} + \sum_n Source(x - nh) \delta(t - t_n)$$

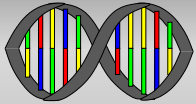


# Fire-Diffuse-Fire-II

Recall that the solution of the heat equation with  $\delta$ -function initial data at  $x = x_0$  and at  $t = t_0$  is

$$u(x, t) = \frac{1}{\sqrt{4\pi(t - t_0)}} \exp\left(-\frac{(x - x_0)^2}{4D(t - t_0)}\right)$$



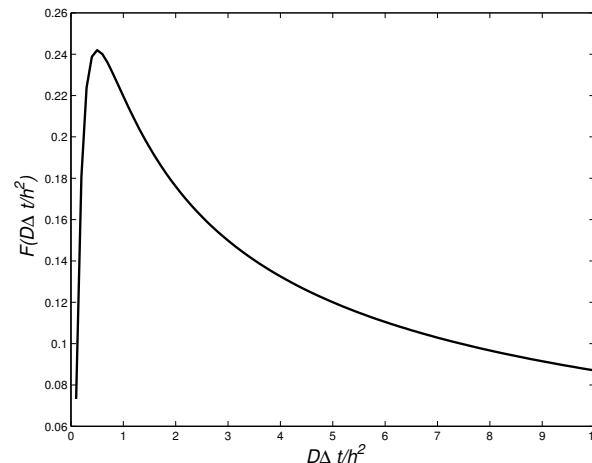


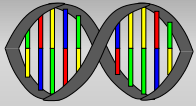
# Fire-Diffuse-Fire-III

Suppose known firing times are  $t_j$  at position  $x_j = jh$ ,  
 $j = -\infty, \dots, n-1$ . Find  $t_n$ . At  $x = x_n = nh$ ,

$$u(nh, t) = \sum_{j=-\infty}^{n-1} \frac{C}{\sqrt{4\pi(t-t_j)}} \exp\left(-\frac{(nh-jh)^2}{4D(t-t_j)}\right)$$

$$\approx \frac{C}{\sqrt{4\pi(t-t_{n-1})}} \exp\left(-\frac{h^2}{4D(t-t_{n-1})}\right) = \frac{C}{h} f\left(\frac{D\Delta t}{h^2}\right)$$



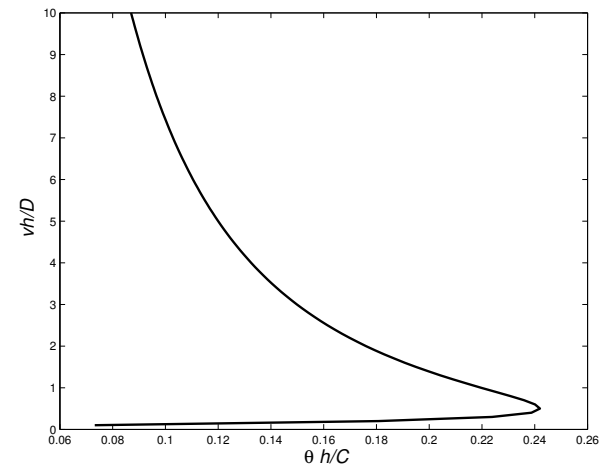
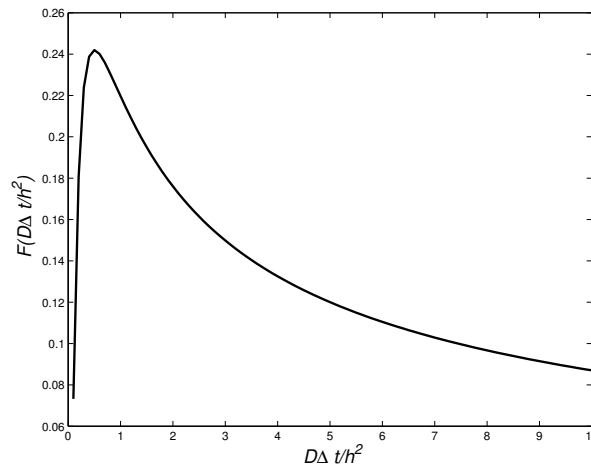


# Fire-Diffuse-Fire-IV

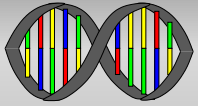
Solve the equation

$$\frac{\theta h}{C} = f\left(\frac{D\Delta t}{h^2}\right)$$

This is easy to do graphically:



Conclusion: Propagation fails for  $\frac{\theta h}{C} > \theta^* \approx 0.25$  (i.e. if  $h$  is too large,  $\theta$  is too large, or  $C$  is too small.)



# ***With Recovery***

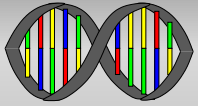
Including recovery variables

$$\frac{\partial v}{\partial t} = D \frac{\partial^2 v}{\partial x^2} + f(v, w), \quad \frac{\partial w}{\partial t} = g(v, w)$$

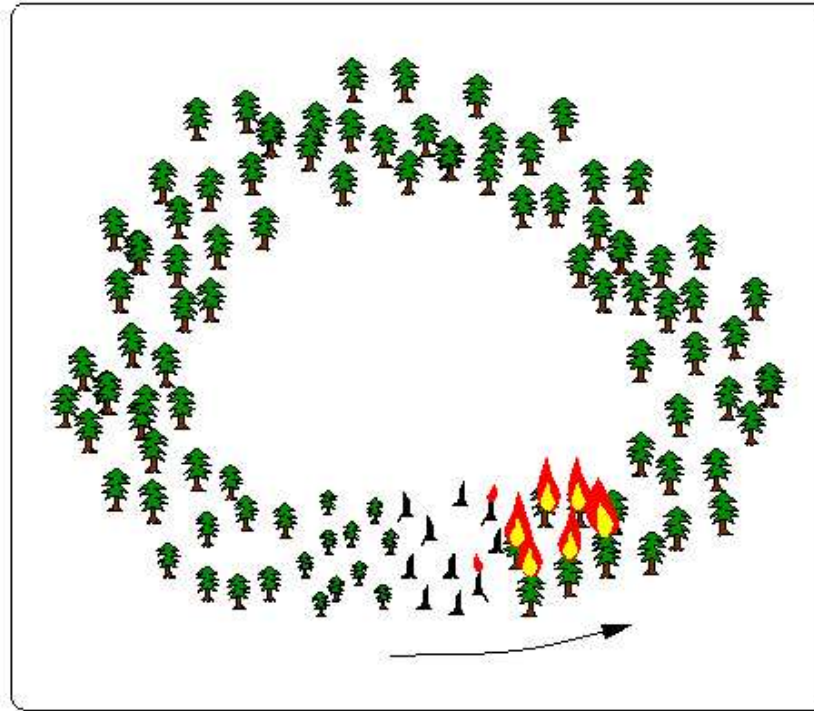
Solitary Pulse

Periodic Waves

Skipped Beats



# *Periodic Ring*



To be continued ...