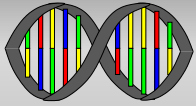


Introduction to Physiology III - Excitability

J. P. Keener

Mathematics Department
University of Utah

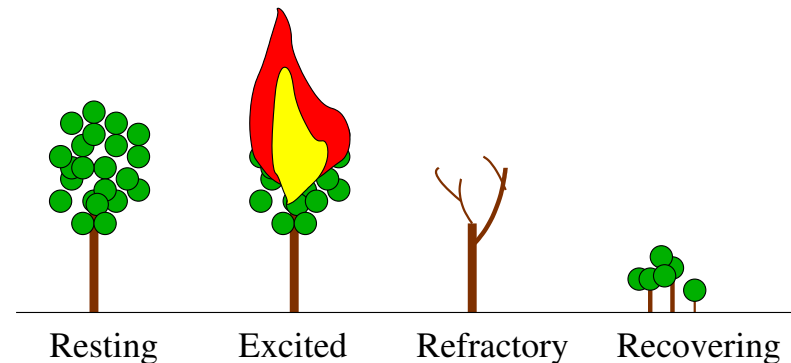


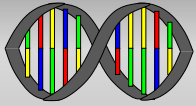
Examples of Excitable Media

- CICR (Calcium Induced Calcium Release)
- Nerve cells
- cardiac cells, muscle cells
- Slime mold (*dictyostelium discoideum*)
- B-Z reagent
- Forest Fires

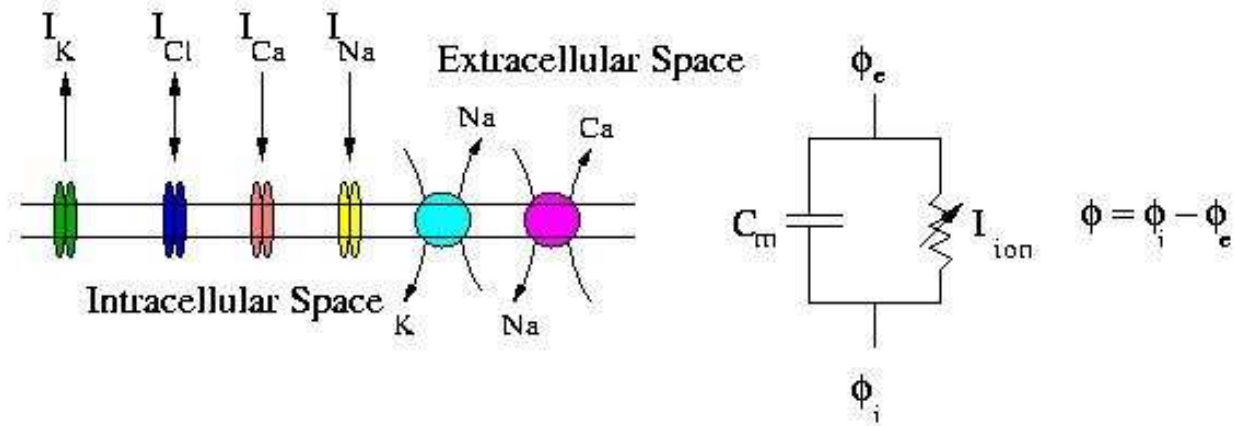
Features of Excitability

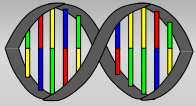
- Threshold Behavior
- Refractoriness
- Recovery



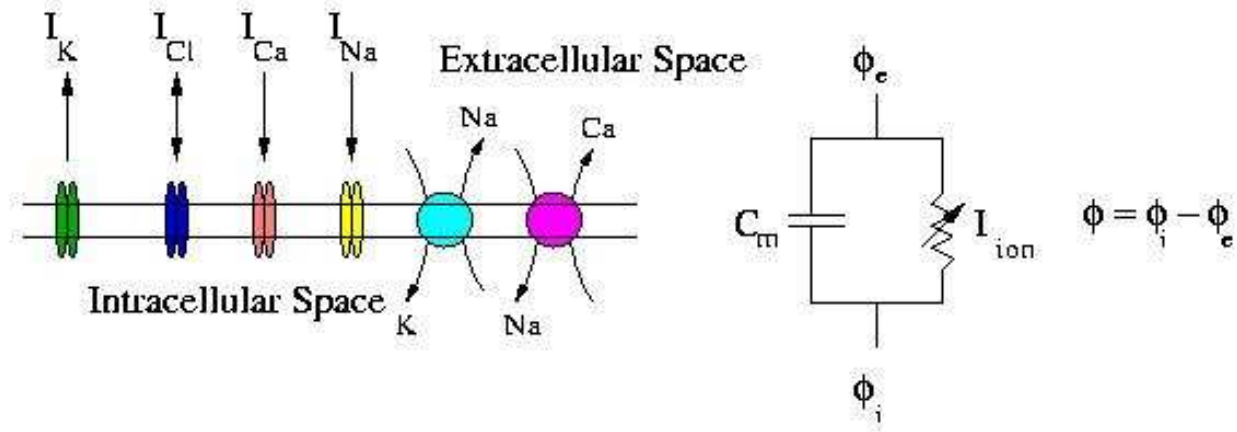


Modeling Membrane Electrical Activity



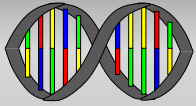


Modeling Membrane Electrical Activity



Transmembrane potential ϕ is regulated by transmembrane ionic currents and capacitive currents:

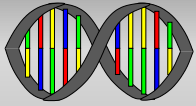
$$C_m \frac{d\phi}{dt} + I_{ion}(\phi, w) = I_{in} \quad \text{where} \quad \frac{dw}{dt} = g(\phi, w), \quad w \in R^n$$



Examples

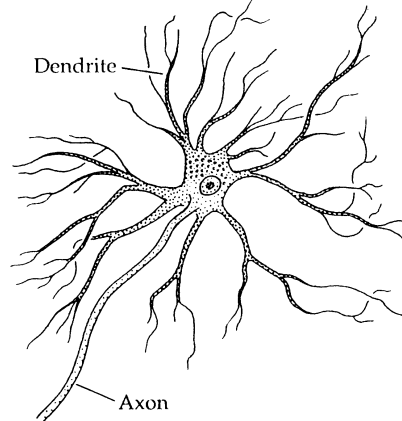
Examples include:

- Neuron - **Hodgkin-Huxley model**
- Purkinje fiber - Noble
- Cardiac cells - Beeler-Reuter, Luo-Rudy, Winslow-Jafri, Bers
- Two Variable Models - **reduced HH, FitzHugh-Nagumo, Mitchell-Schaeffer, Morris-Lecar, McKean, Puschino, etc.)**

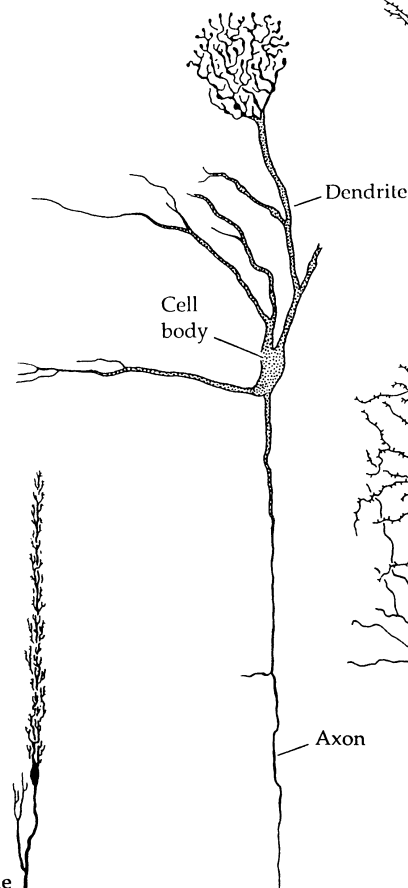


The Squid Giant Axon...

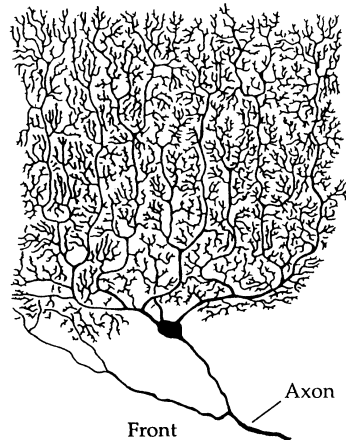
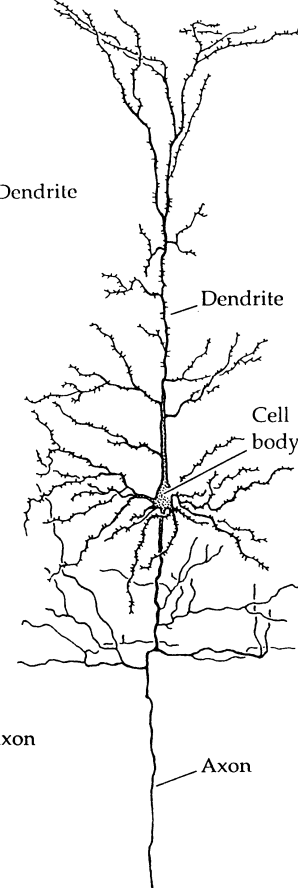
MOTOR NEURON
FROM SPINAL CORD



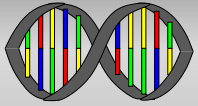
MITRAL CELL FROM
OLFACTORY BULB



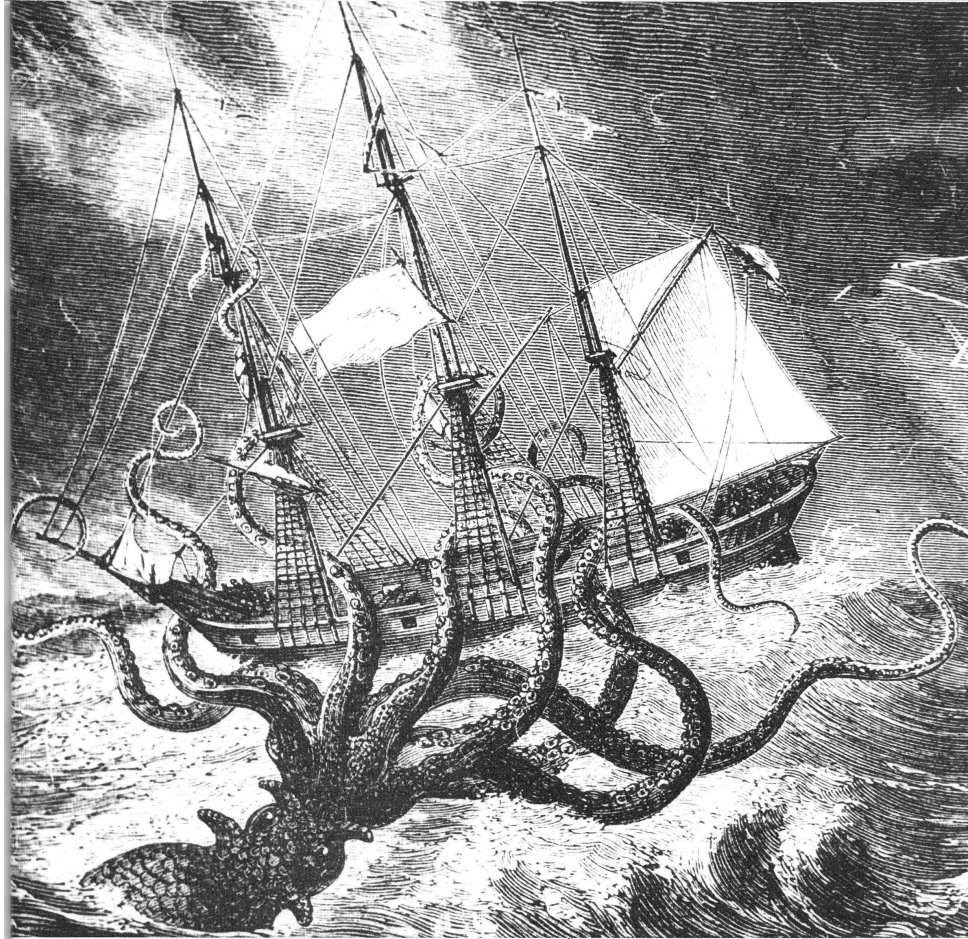
PYRAMIDAL CELL
FROM CORTEX

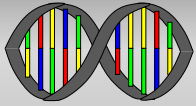


PURKINJE CELL

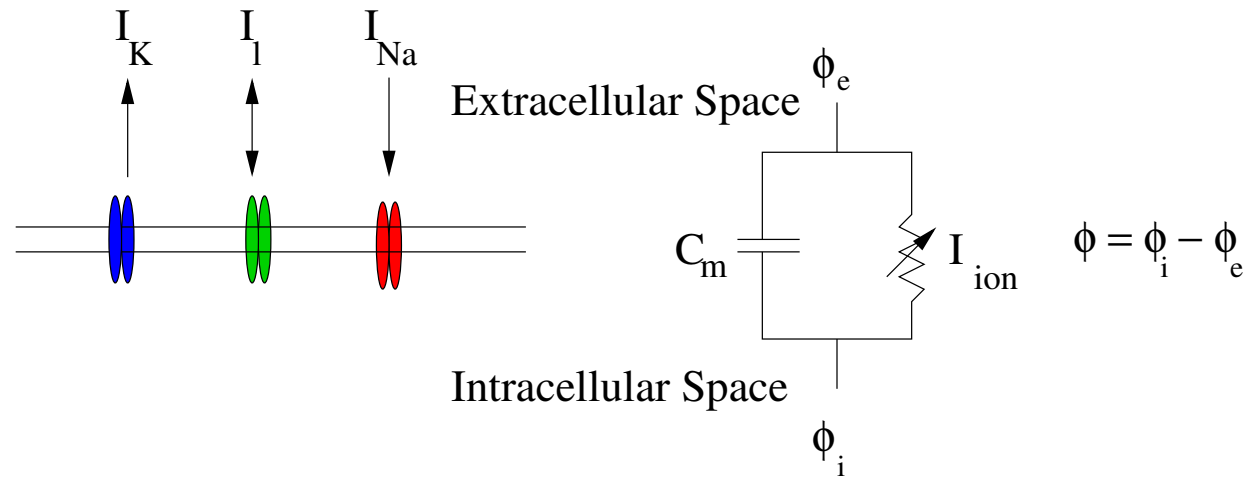


is not the Giant Squid Axon

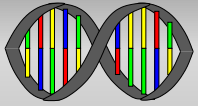




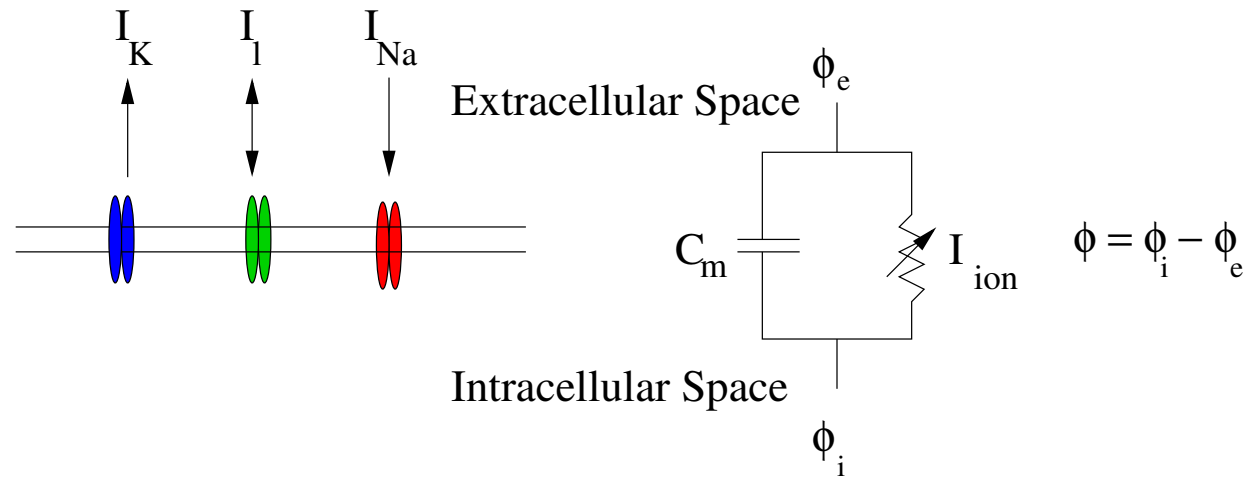
The Hodgkin-Huxley Equations



$$C_m \frac{dV}{dt} + I_{Na} + I_K + I_l = 0,$$

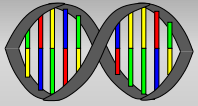


The Hodgkin-Huxley Equations

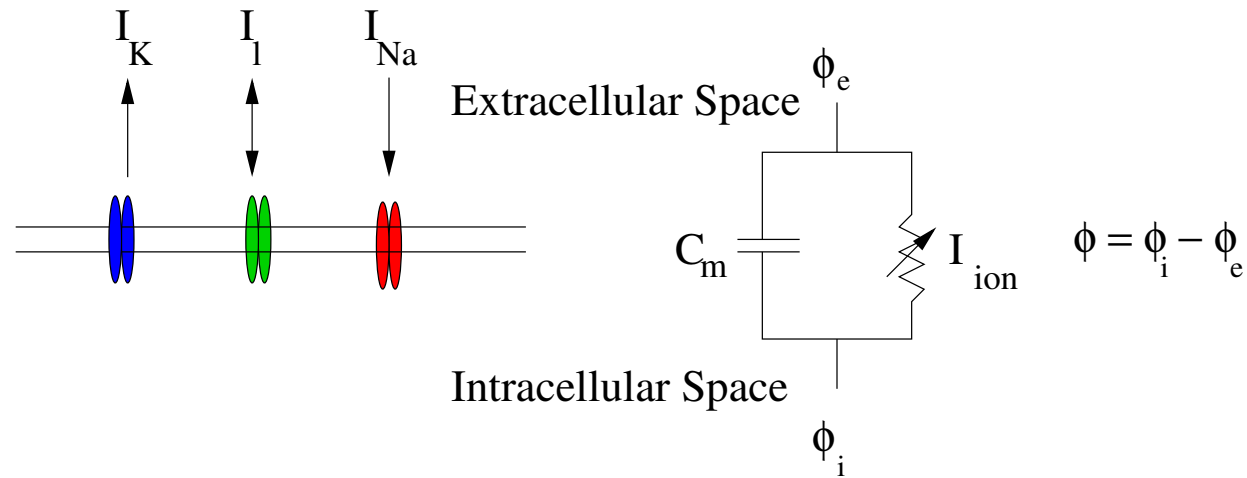


$$C_m \frac{dV}{dt} + \boxed{I_{Na}} + I_K + I_l = 0,$$

with sodium current I_{Na} ,

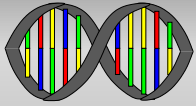


The Hodgkin-Huxley Equations

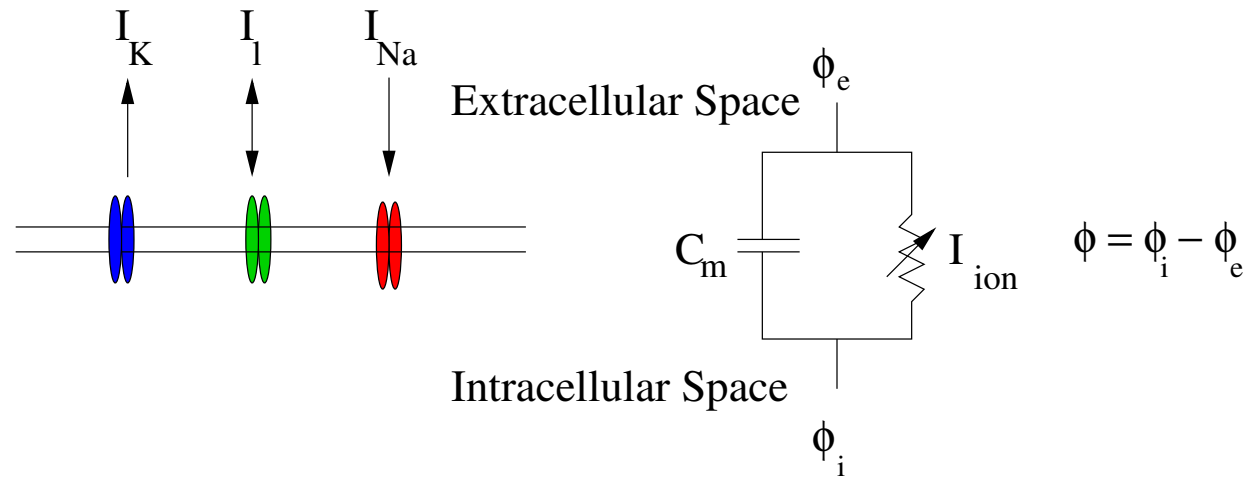


$$C_m \frac{dV}{dt} + \boxed{I_{Na}} + \boxed{I_K} + I_l = 0,$$

with **sodium current** I_{Na} , **potassium current** I_K ,

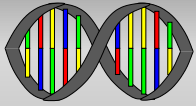


The Hodgkin-Huxley Equations



$$C_m \frac{dV}{dt} + I_{Na} + I_K + I_l = 0,$$

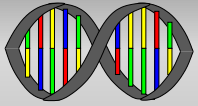
with sodium current I_{Na} , potassium current I_K , and leak current I_l .



Ionic Currents

Ionic currents are typically of the form

$$I = g(\phi, t) \Phi(\phi)$$

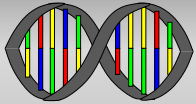


Ionic Currents

Ionic currents are typically of the form

$$I = \boxed{g(\phi, t)} \Phi(\phi)$$

where $g(\phi, t)$ is the total number of open channels,

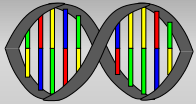


Ionic Currents

Ionic currents are typically of the form

$$I = g(\phi, t) \Phi(\phi)$$

where $g(\phi, t)$ is the total number of open channels, and $\Phi(\phi)$ is the I - ϕ relationship for a single channel.



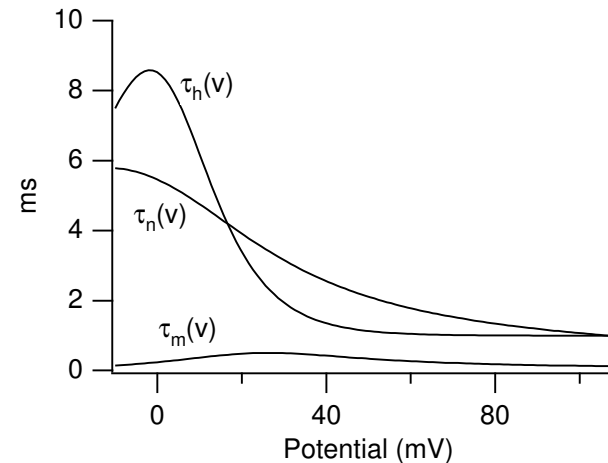
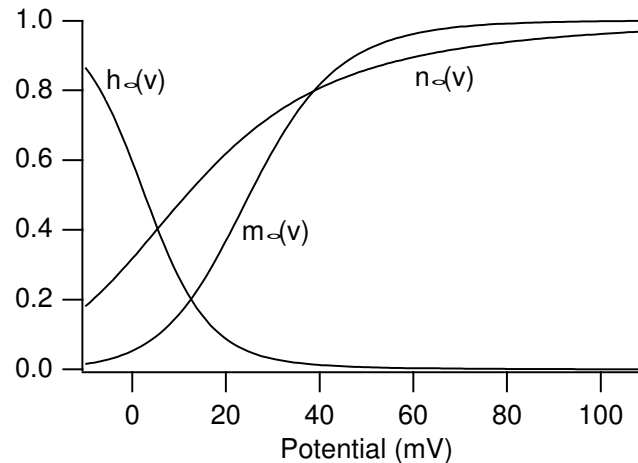
Currents

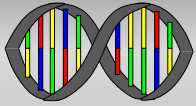
Hodgkin and Huxley found that

$$I_k = g_k n^4 (\phi - \phi_K), \quad I_{Na} = g_{Na} m^3 h (\phi - \phi_{Na}),$$

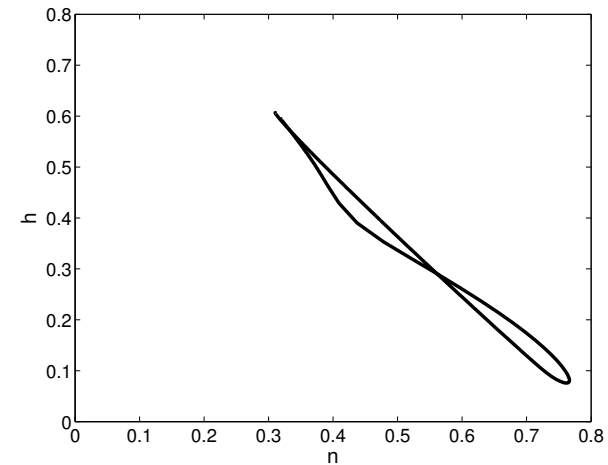
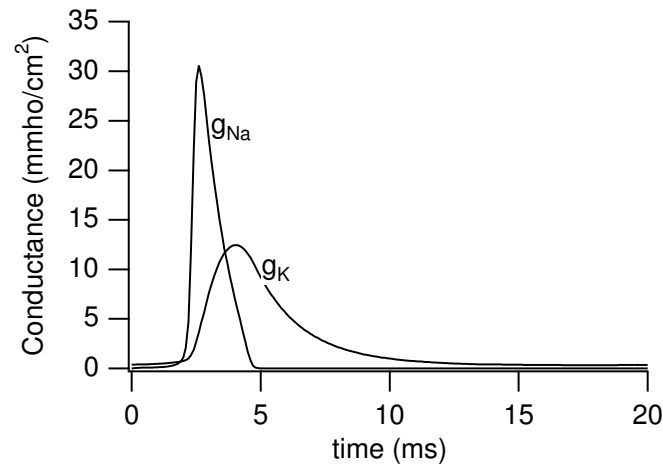
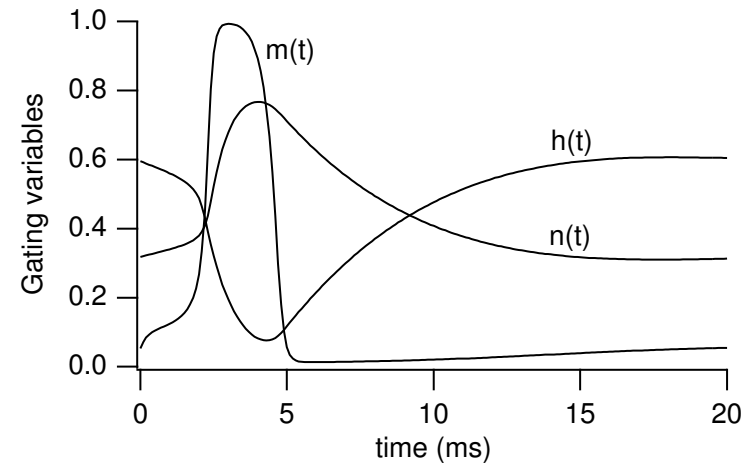
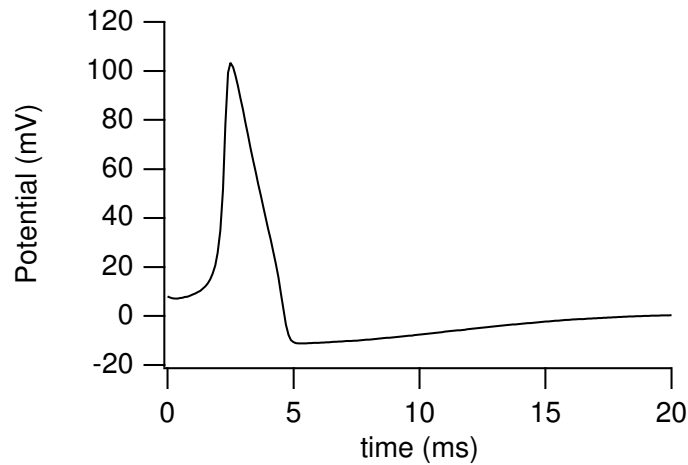
where

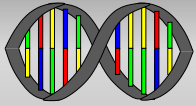
$$\tau_u(\phi) \frac{du}{dt} = u_\infty(\phi) - u, \quad u = m, n, h$$





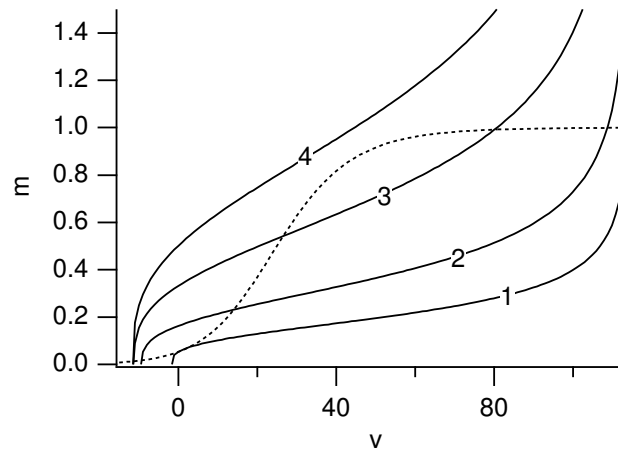
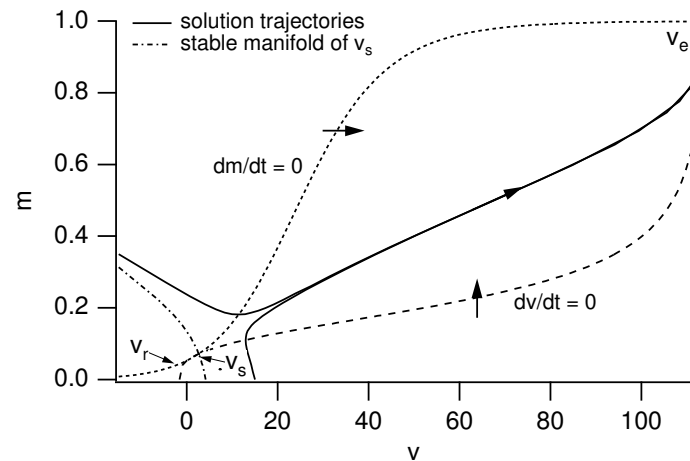
Action Potential Dynamics

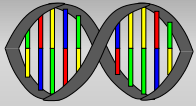




Fast-Slow Subsystem Dynamics

Observe that $\tau_m \ll \tau_n, \tau_h$



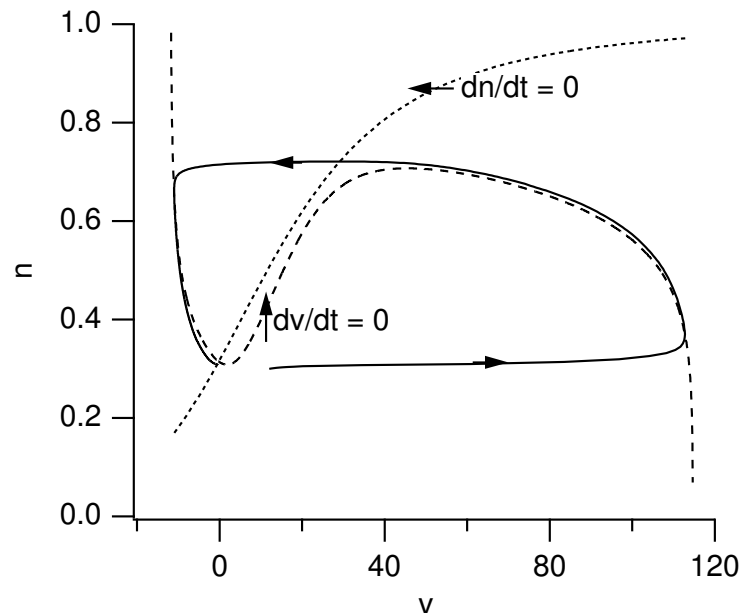


Two Variable Reduction of HH Eqns

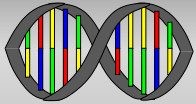
Set $m = m_\infty(\phi)$, and set $h + n \approx N = 0.85$.
This reduces to a two variable system

$$C \frac{d\phi}{dt} = \bar{g}_K n^4 (\phi - \phi_K) + \bar{g}_{Na} m_\infty^3(\phi) (N - n) (\phi - \phi_{Na}) + \bar{g}_l (\phi - \phi_L),$$

$$\tau_n(\phi) \frac{dn}{dt} = n_\infty(\phi) - n.$$



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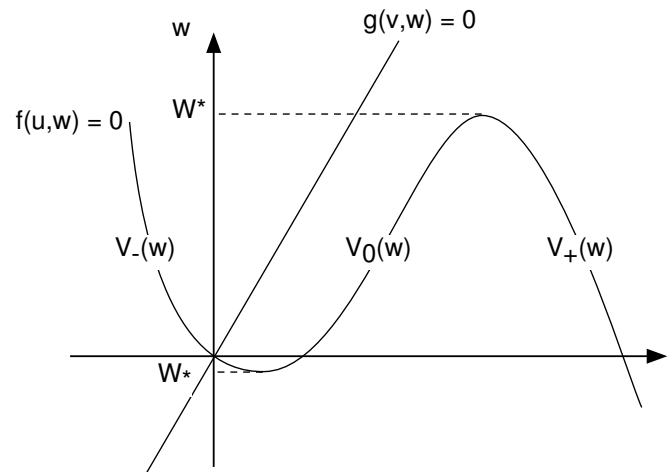
Two Variable Models

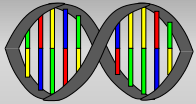
Following is a summary of two variable models of excitable media. The models described here are all of the form

$$\frac{dv}{dt} = f(v, w) + I$$

$$\frac{dw}{dt} = g(v, w)$$

Typically, v is a “fast” variable, while w is a “slow” variable.





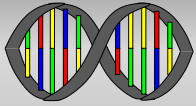
Cubic FitzHugh-Nagumo

The model that started the whole business uses a cubic polynomial (a variant of the van der Pol equation).

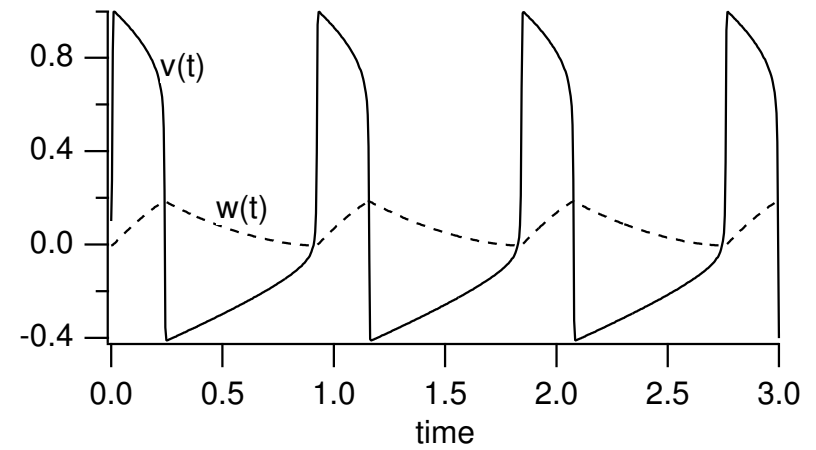
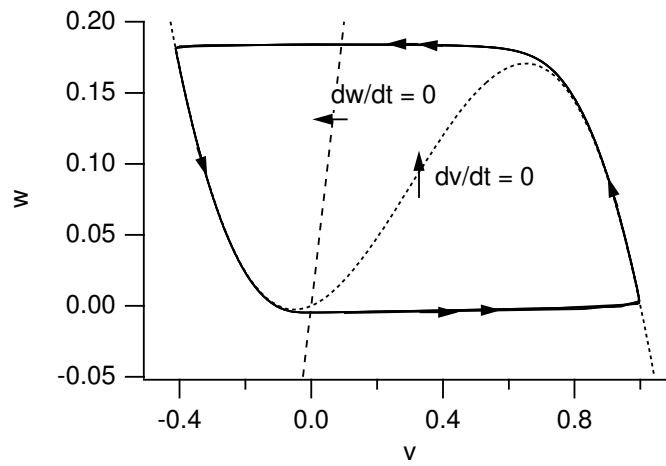
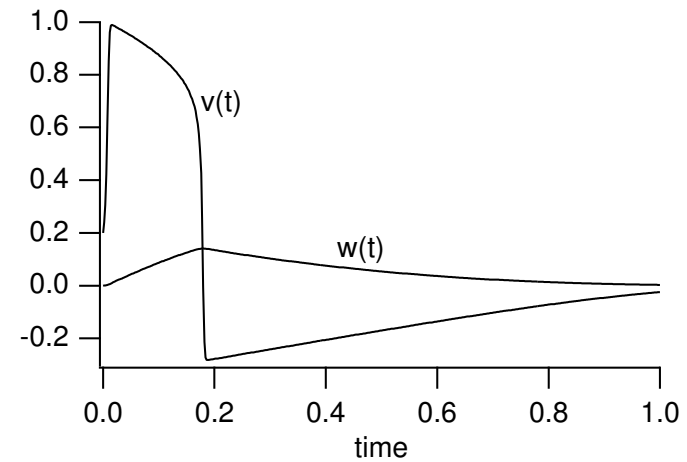
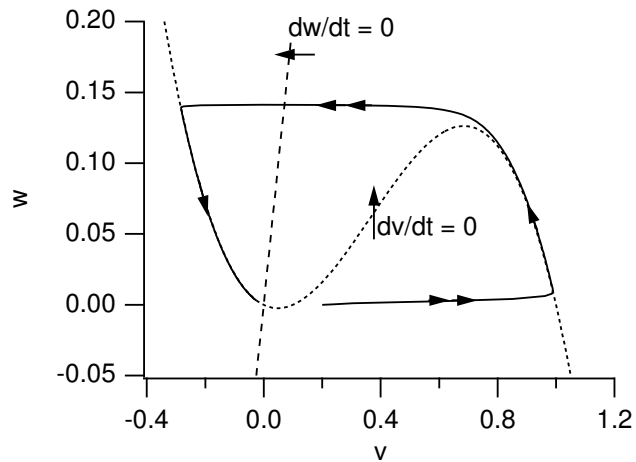
$$F(v, w) = Av(v - \alpha)(1 - v) - w,$$

$$G(v, w) = \epsilon(v - \gamma w).$$

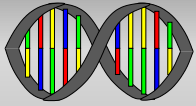
with $0 < \alpha < \frac{1}{2}$, and ϵ “small”.



FitzHugh-Nagumo Equations



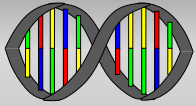
(Go Back)



Mitchell-Schaeffer two-variable model (also in a slightly different but equivalent form by Karma)

$$F(v, w) = \frac{1}{\tau_{in}} w v^2 (1 - v) - \frac{v}{\tau_{out}},$$
$$G(v, w) = \begin{cases} \frac{1}{\tau_{open}} (1 - w) & v < v_{gate} \\ -\frac{w}{\tau_{close}} & v > v_{gate} \end{cases}$$

Notice that $F(v, w)$ is cubic in v , and w is an inactivation variable (like h in HH).



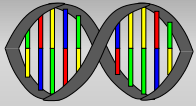
Mitchell-Schaeffer Revised

To make the Mitchell-Schaeffer look like an ionic model, take

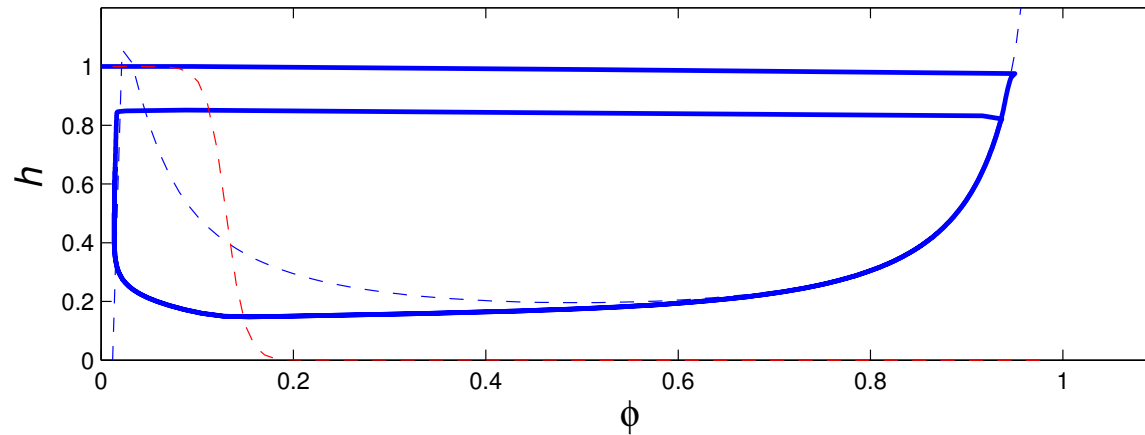
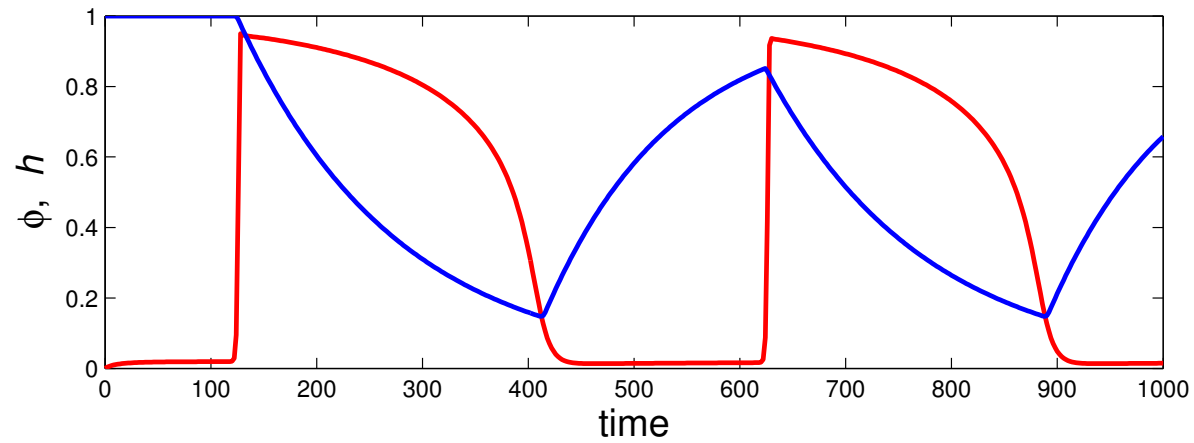
$$\begin{aligned} C_m \frac{dv}{dt} &= g_{Na} h m^2 (V_{Na} - v) + g_K (V_K - v), \\ \tau_h \frac{dh}{dt} &= h_\infty(v) - h \end{aligned}$$

where

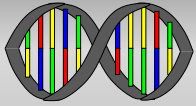
$$m(v) = \begin{cases} 0, & v < 0 \\ v, & 0 < v < 1 \\ 1, & v > 1 \end{cases}, \quad \begin{aligned} h_\infty &= 1 - f(v), \\ \tau_h &= \tau_{open} + (\tau_{close} - \tau_{open}) f(v) \\ f(v) &= \frac{1}{2}(1 + \tanh(\kappa(v - v_{gate}))), \end{aligned}$$



Mitchell-Schaeffer Revised-II



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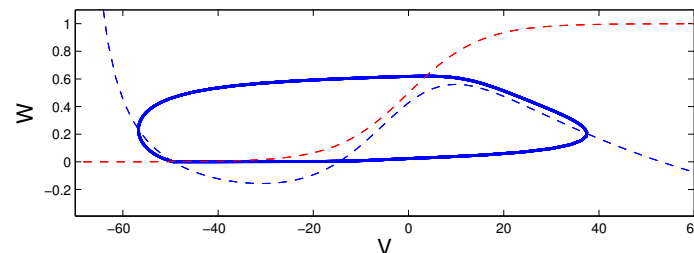
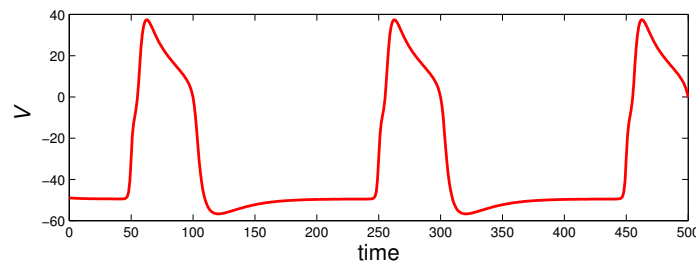
Morris-Lecar

This model was devised for barnacle muscle fiber.

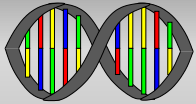
$$F(v, w) = -g_{ca}m_{\infty}(v)(v - v_{ca}) - g_k w(v - v_k) - g_l(v - v_l) + I_{app}$$

$$G(v, w) = \phi \cosh\left(\frac{1}{2} \frac{v - v_3}{v_4}\right)(w_{\infty}(v) - w),$$

$$m_{\infty}(v) = \frac{1}{2} + \frac{1}{2} \tanh\left(\frac{v - v_1}{v_2}\right), \quad w_{\infty}(v) = \left(1 + \tanh\left(\frac{v - v_3}{2v_4}\right)\right).$$

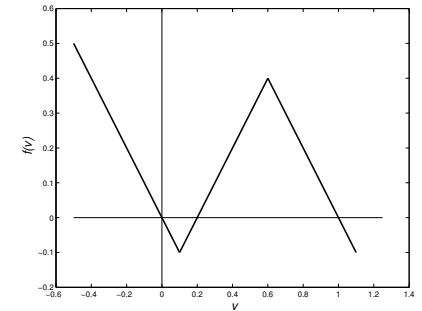


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McKean suggested two piecewise linear models with $F(v, w) = f(v) - w$ and $G(v, w) = \epsilon(v - \gamma w)$. For the first,

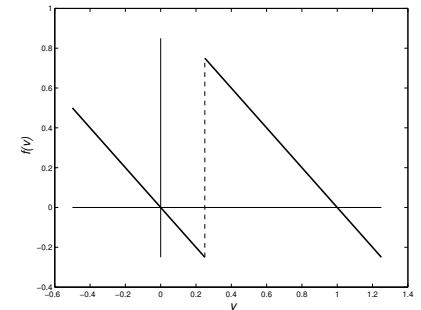
$$f(v) = \begin{cases} -v & v < \frac{\alpha}{2} \\ v - \alpha & \frac{\alpha}{2} < v < \frac{1+\alpha}{2} \\ 1 - v & v > \frac{1+\alpha}{2} \end{cases}$$



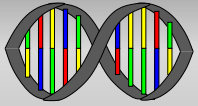
where $0 < \alpha < \frac{1}{2}$.

The second model suggested by McKean had

$$f(v) = \begin{cases} -v & v < \alpha \\ 1 - v & v > \alpha \end{cases}$$



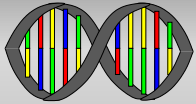
and $\gamma = 0$.



A model devised to give very fast 2D computations (the code is known as EZspiral)

$$F(v, w) = v(1 - v)\left(v - \frac{w + b}{a}\right),$$

$$G(v, w) = \epsilon(v - w).$$

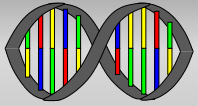


These dynamics describe the oxidation-reduction of malonic acid. For this system,

$$F(v, w) = v - v^2 - (fw + \phi_0) \frac{v - q}{v + q} \quad (-9)$$

$$G(v, w) = \epsilon(v - w) \quad (-9)$$

with typical parameter values $\epsilon = 0.05$, $q = 0.002$, $f = 3.5$, $\phi_0 = 0.01$.

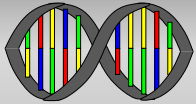


Features of Excitable Systems

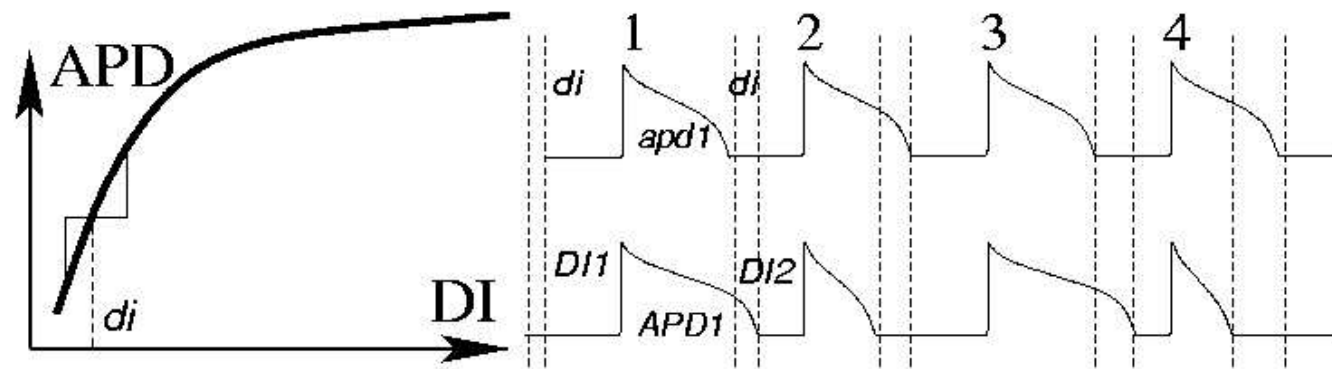
Threshold Behavior, Refractoriness

Alternans

Wenckebach Patterns



APD Alternans



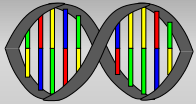
Action Potential Duration Restitution Curve

$$APD_n + DI_n = BCL.$$

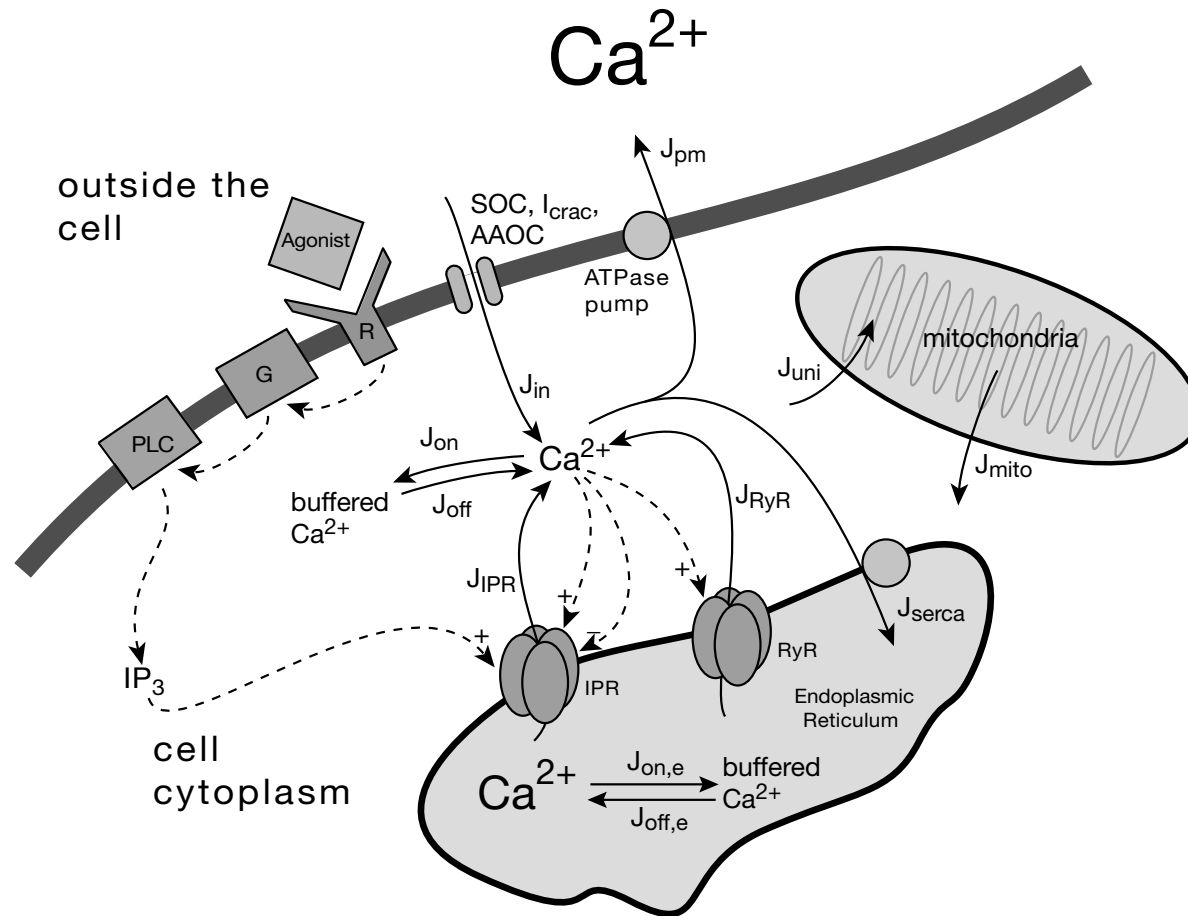
where $APD_n = A(DI_{n-1})$ is the restitution curve. It follows that

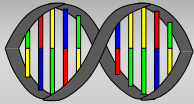
$$DI_n = BCL - A(DI_{n-1}),$$

APD Map Animated



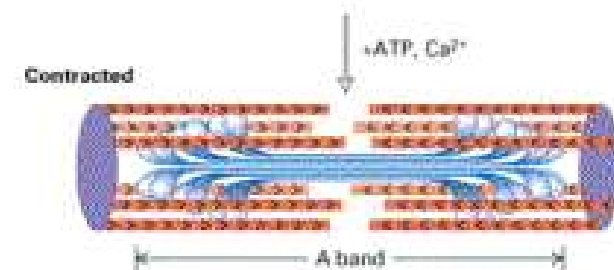
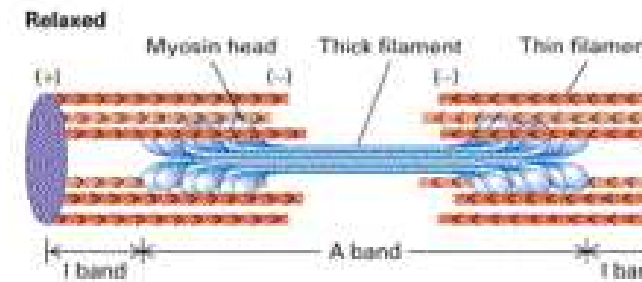
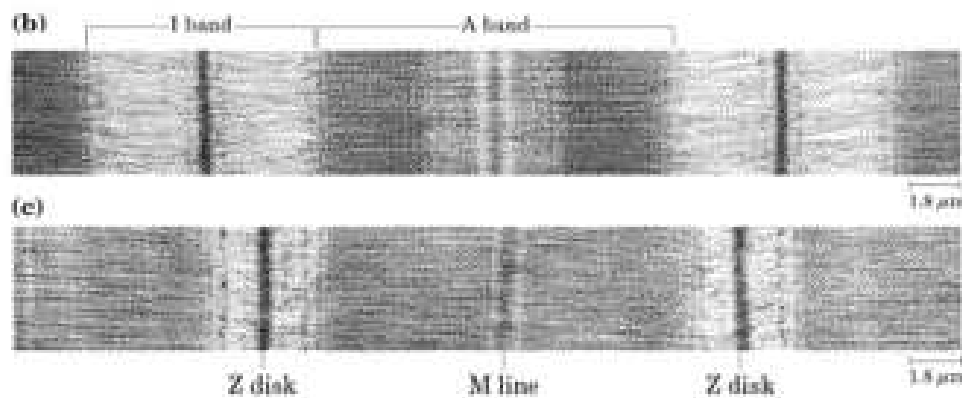
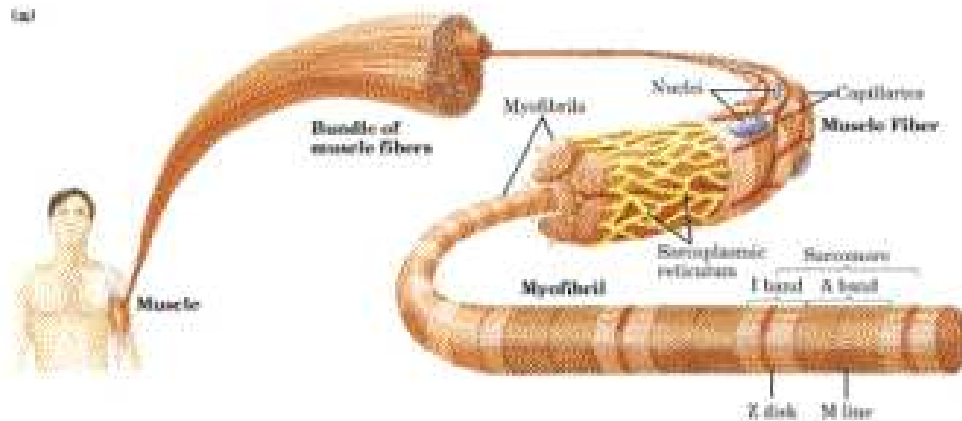
Intracellular Calcium

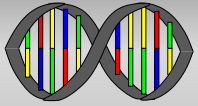




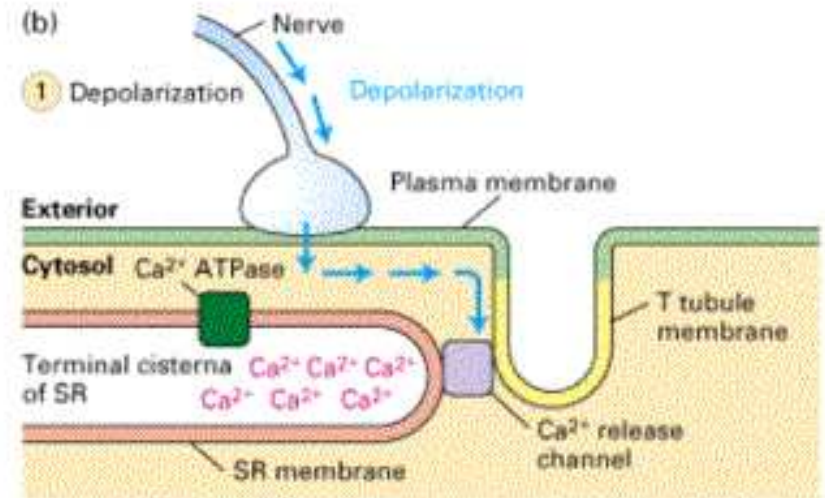
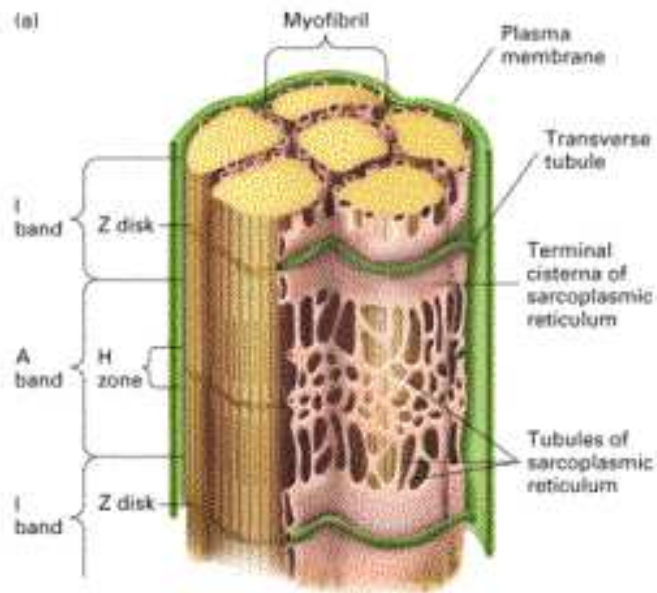
Muscle

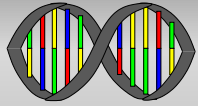
Structure of skeletal muscle





Muscle - II

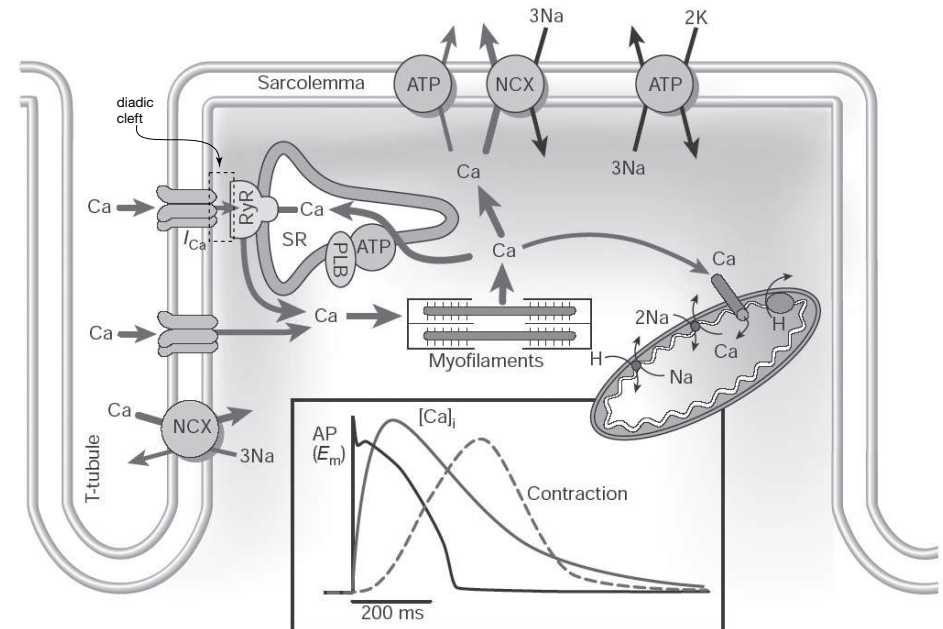


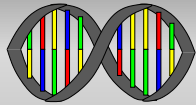


Excitation-Contraction Coupling

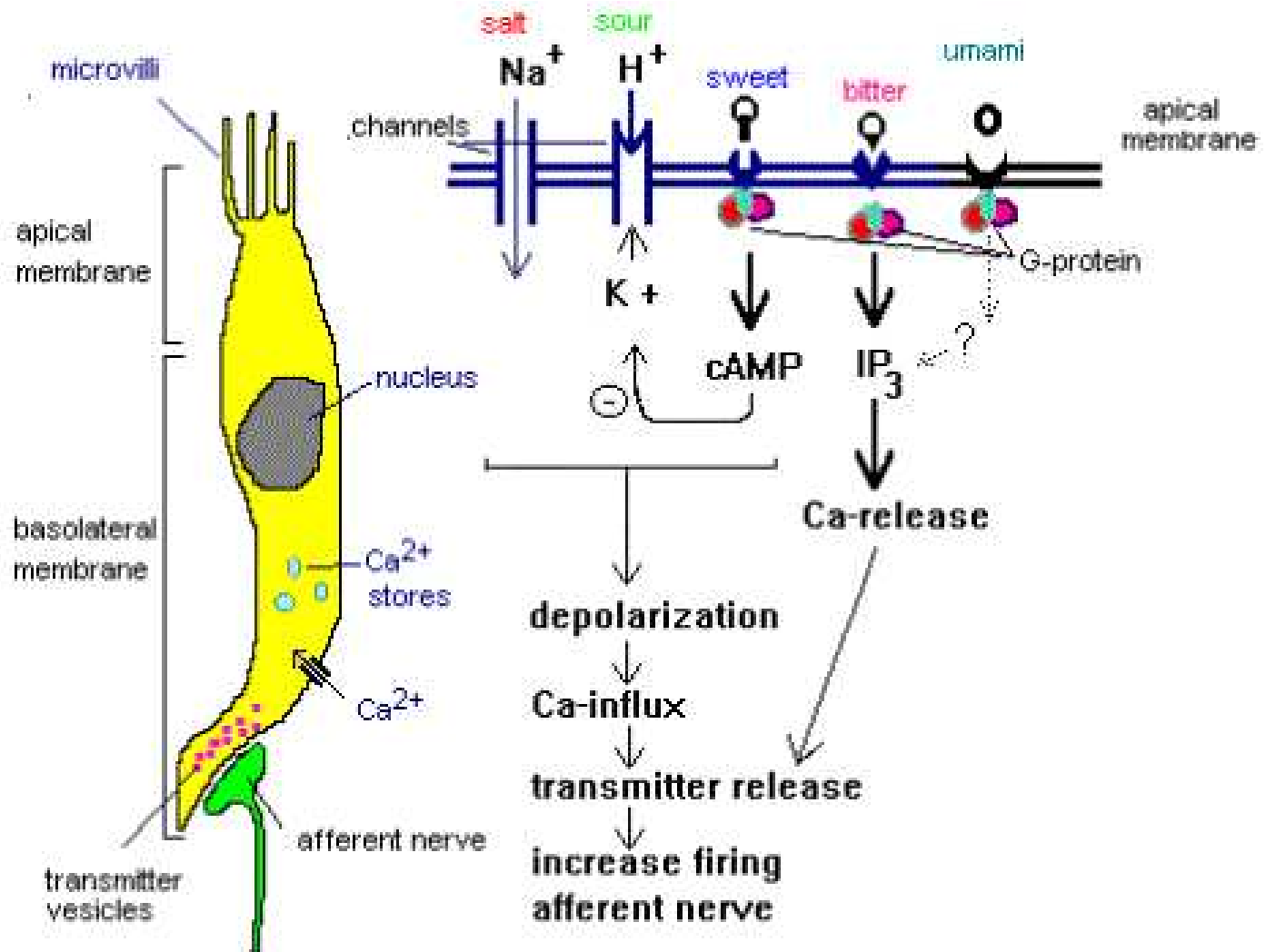
Cardiac cells are interesting because they contain TWO excitable systems that are interconnected

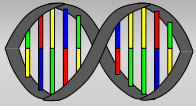
- The sodium-potassium electrical action potential, that stimulates an inward calcium flux
- which excites CICR
- which causes muscles to contract.



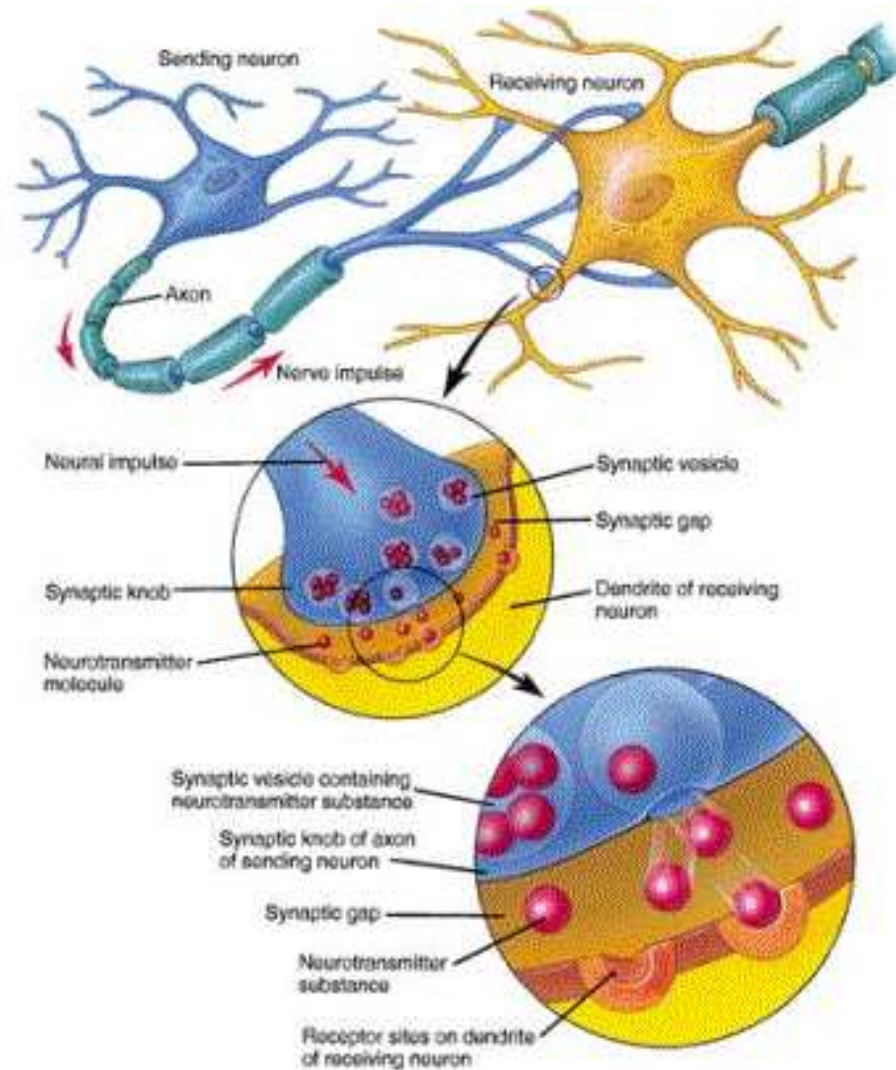


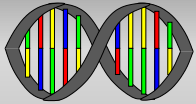
Taste Buds



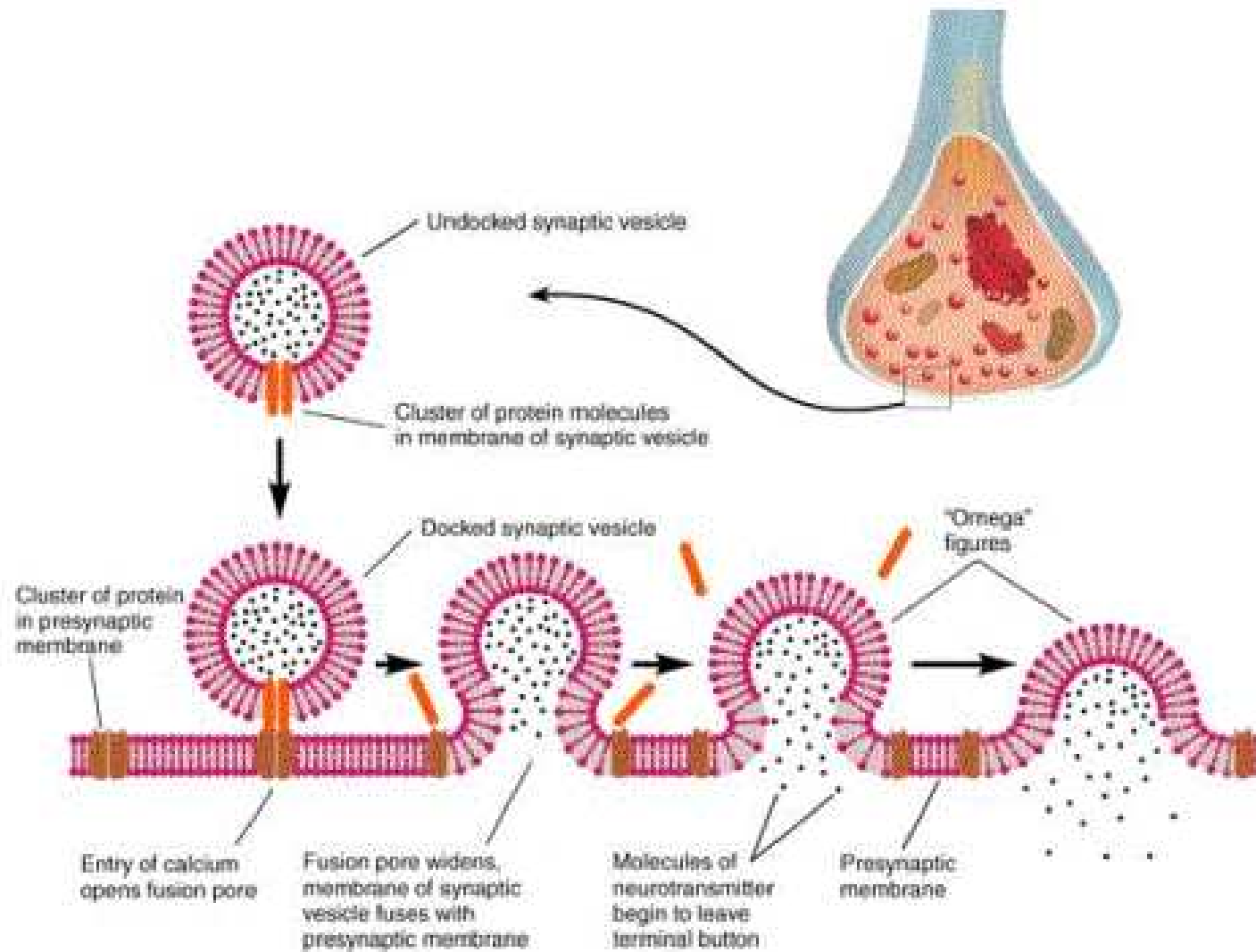


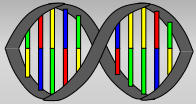
Neural Synapses



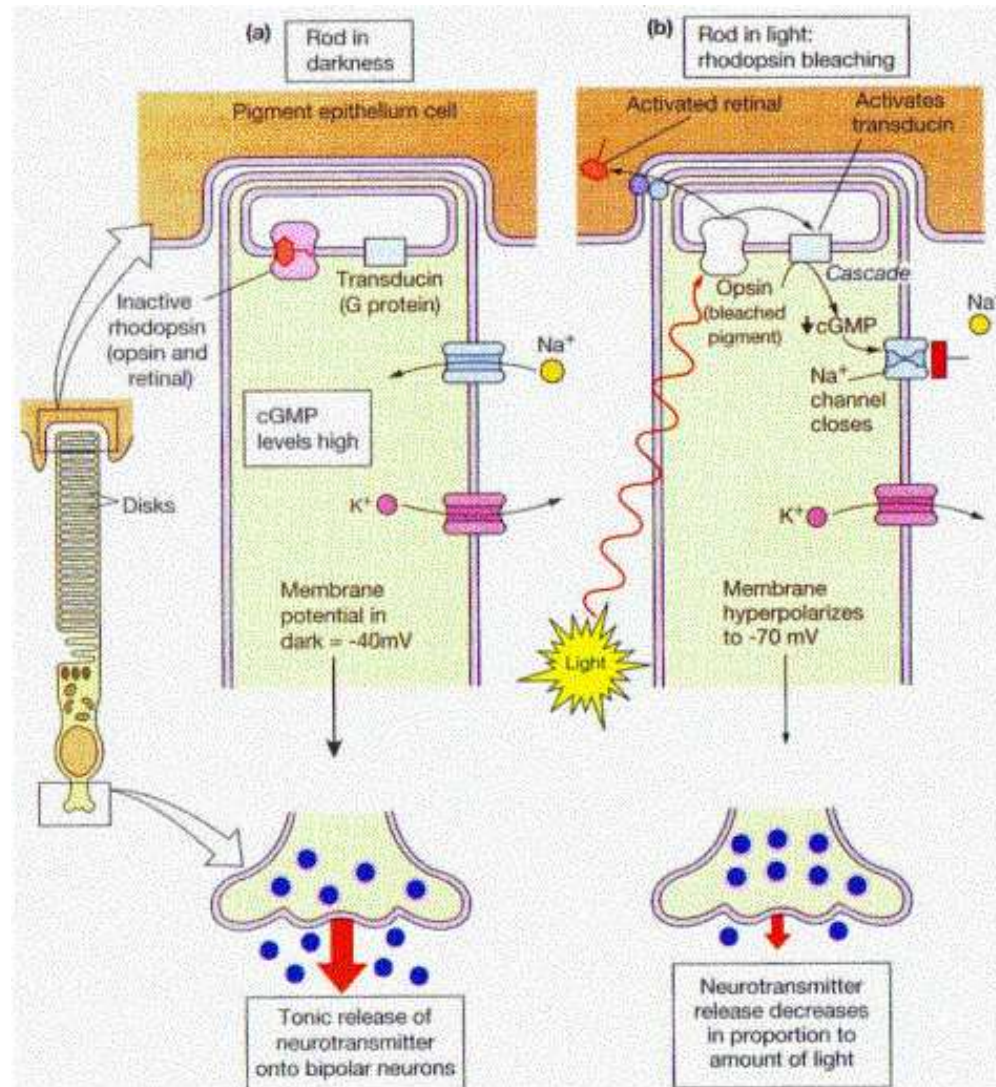


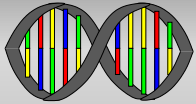
Neurotransmitter - II



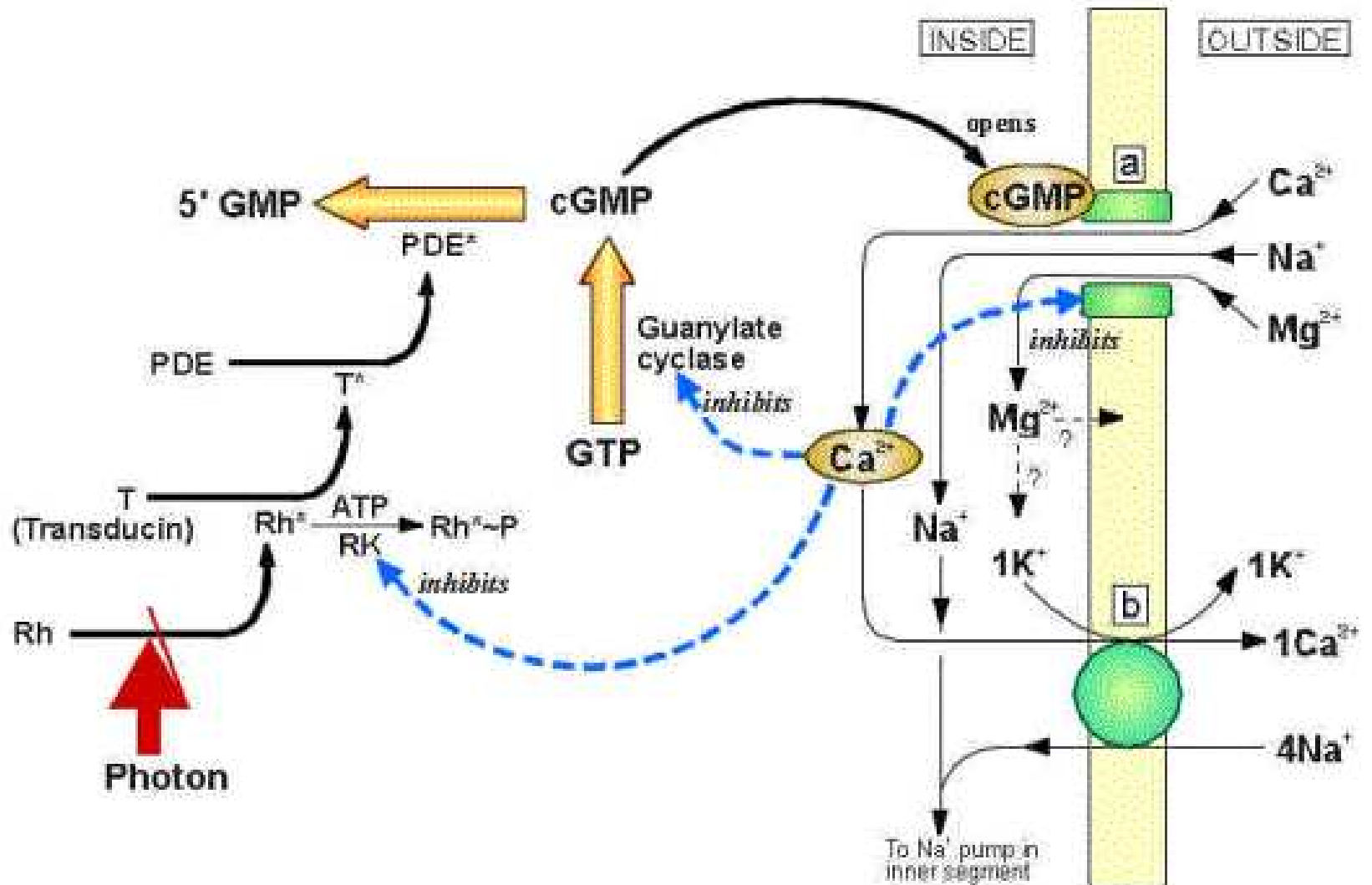


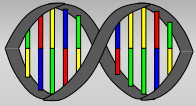
Phototransduction





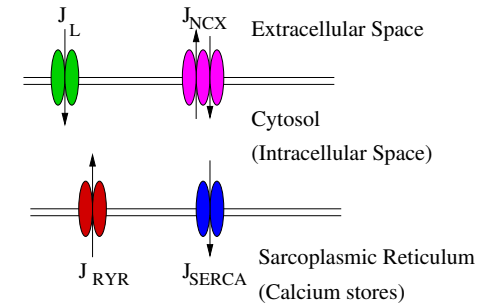
Phototransduction

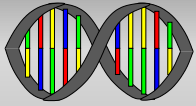




Calcium Handling

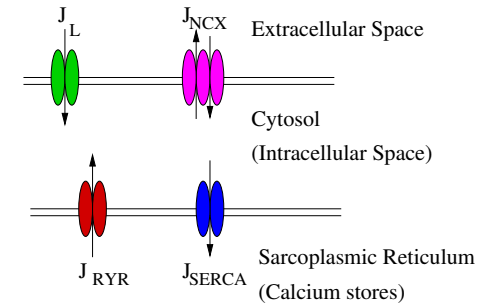
$$v \frac{dc}{dt} = J_{R\bar{Y}R} - J_{S\bar{E}R\bar{C}A} + J_L - J_{N\bar{C}X}$$





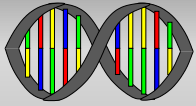
Calcium Handling

$$v \frac{dc}{dt} = J_{R\text{YR}} - J_{SERCA} + J_L - J_{NCX}$$



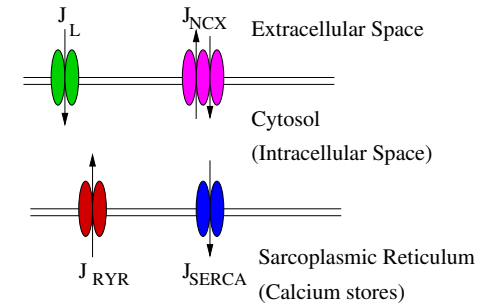
with

$J_{R\text{YR}}$ Ryanodine Receptor - calcium regulated calcium channel,



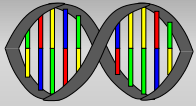
Calcium Handling

$$v \frac{dc}{dt} = J_{RYR} - J_{SERCA} + J_L - J_{NCX}$$



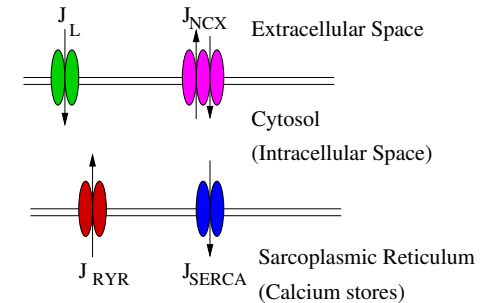
with

J_{RYR} Ryanodine Receptor - calcium regulated calcium channel,
 J_{SERCA} Sarco- and Endoplasmic Reticulum Calcium ATPase,



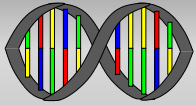
Calcium Handling

$$v \frac{dc}{dt} = J_{RYR} - J_{SERCA} + J_L - J_{NCX}$$



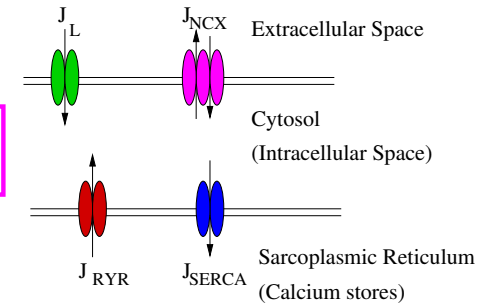
with

J_{RYR} Ryanodine Receptor - calcium regulated calcium channel,
 J_{SERCA} Sarco- and Endoplasmic Reticulum Calcium ATPase,
 J_L L-type voltage regulated calcium channel,



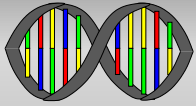
Calcium Handling

$$v \frac{dc}{dt} = J_{RYR} - J_{SERCA} + J_L - J_{NCX}$$



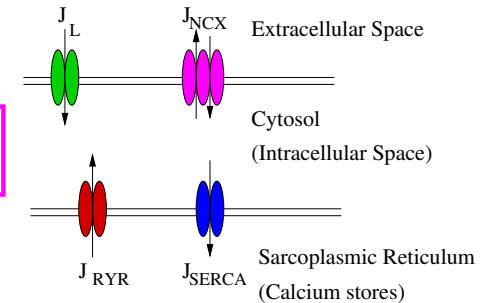
with

J_{RYR} Ryanodine Receptor - calcium regulated calcium channel,
 J_{SERCA} Sarco- and Endoplasmic Reticulum Calcium ATPase,
 J_L L-type voltage regulated calcium channel,
 J_{NCX} sodium(Na^{++})- Calcium eXchanger .



Calcium Handling

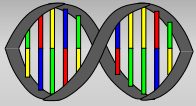
$$v \frac{dc}{dt} = J_{RYR} - J_{SERCA} + J_L - J_{NCX}$$



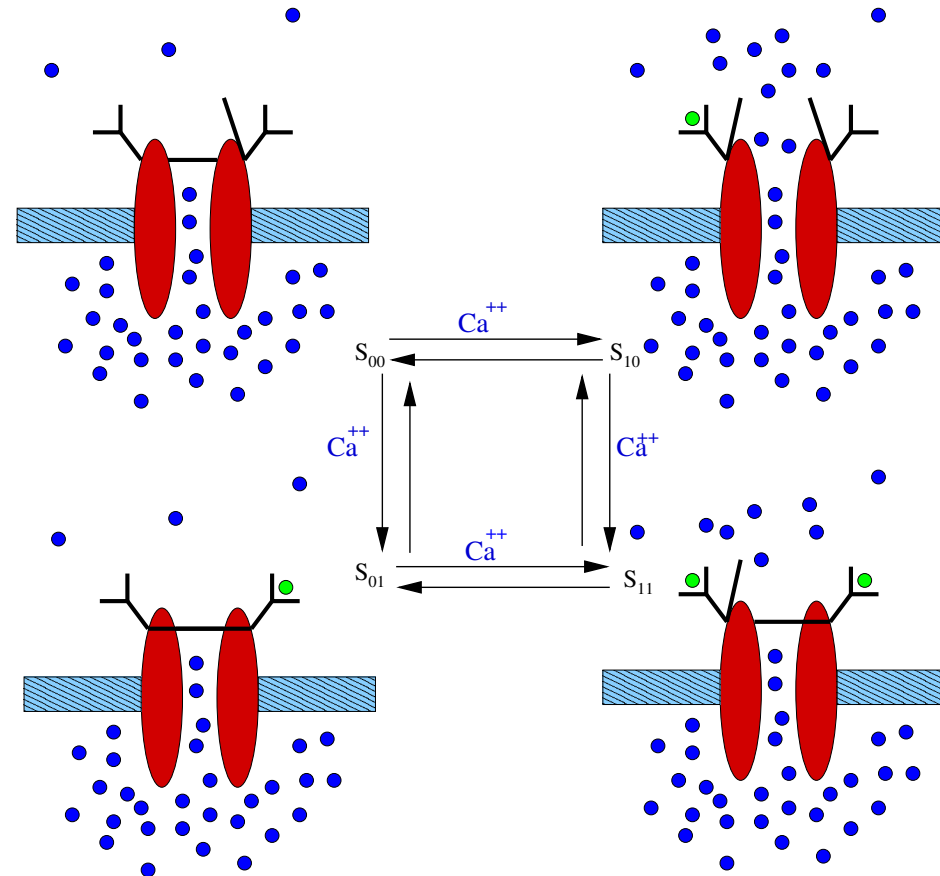
with

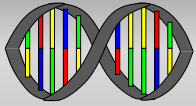
J_{RYR} Ryanodine Receptor - calcium regulated calcium channel,
 J_{SERCA} Sarco- and Endoplasmic Reticulum Calcium ATPase,
 J_L L-type voltage regulated calcium channel,
 J_{NCX} sodium(Na^{++})- Calcium eXchanger .

Challenge: Determine the flux terms.



Ryanodine Receptors





Ryanodine Receptors

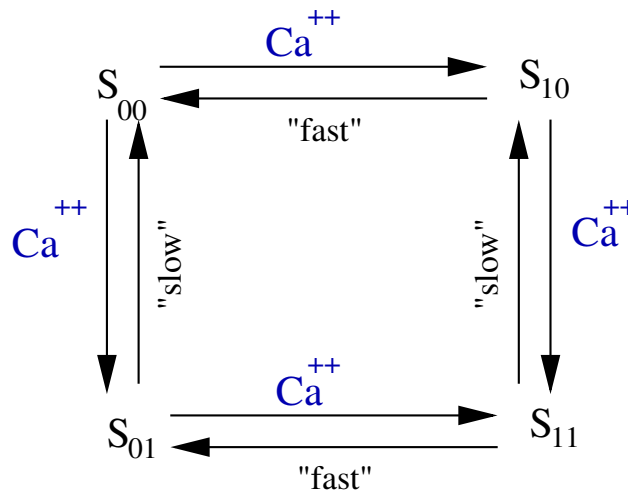
Flux through ryanodine receptor is diffusive,

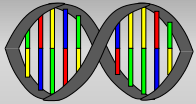
$$J_{RYR} = g_{max} P_o (c - c_{sr})$$

where $P_o = S_{10}^3$ is the open probability. To determine P_o , we must find S_{10} :

$$\frac{dS_{10}}{dt} = k_1 c S_{00} + k_{-2} S_{11} - k_{-1} S_{10} - k_2 c S_{10}$$

and so on.





Observation

If the binding sites are independent (no cooperativity), then

$$S_{10} = mh, S_{00} = (1 - m)h, S_{11} = m(1 - h), S_{01} = (1 - m)(1 - h),$$

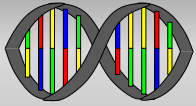
where

$$\frac{dm}{dt} = \phi_m(c)(1 - m) - \psi_m(c)m, \quad \frac{dh}{dt} = \phi_h(c)(1 - h) - \psi(c)h.$$

Furthermore, m is a fast variable, so can be taken to be in qss,

$$m = m_{\infty}(c).$$

Consequently,....



Calcium Dynamics

$$\frac{dc}{dt} = (g_{max}P_o + J_{er})(c_e - c) - J_{SERCA},$$

$$\frac{dh}{dt} = \phi_h(c)(1 - h) - \psi_h(c)h,$$

where

$$J_{SERCA} = V_{max} \frac{c^2}{K_s^2 + c^2},$$

$$P_o = h^3 f(c)$$

